

# CSE 591: GPU Programming

## Case Study: GPU-Accelerated Cone-Beam CT

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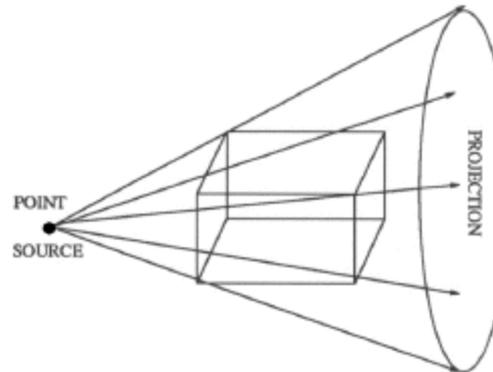
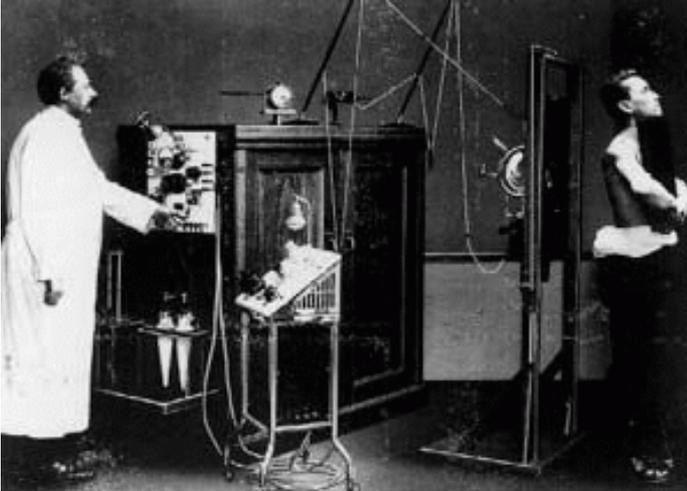
# History: X-Rays

## Wilhelm Conrad Röntgen

- 8 November 1895: discovers X-rays.
- 22 November 1895: X-rays Mrs. Röntgen's hand.
- 1901: receives first Nobel Prize in physics



An early X-ray imaging system:



Note: so far all we can see is a projection across the patient:

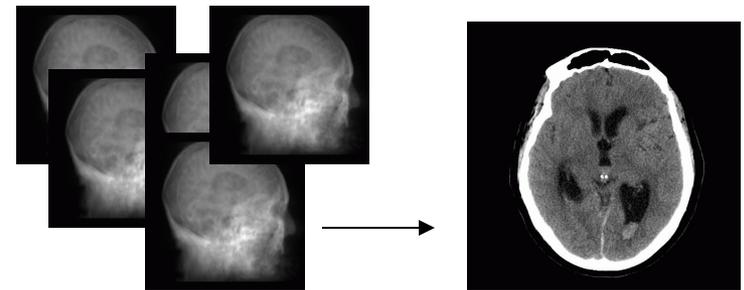
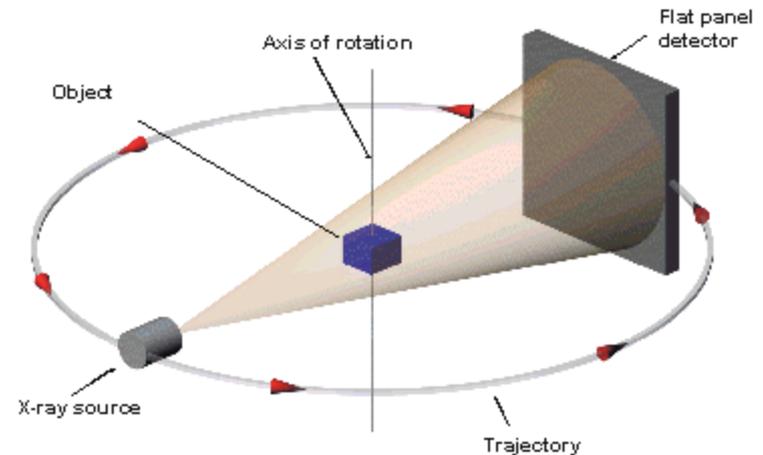
# History: Computed Tomography

## The breakthrough:

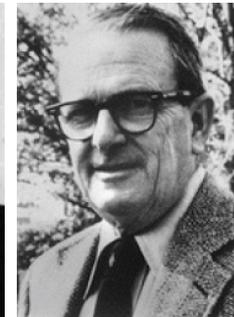
- acquiring many projections around the object enables the reconstruction of the 3D object (or a cross-sectional 2D slice)

## CT reconstruction pioneers:

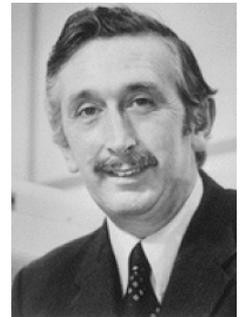
- 1917: Johann Radon establishes the mathematical framework for tomography, now called the Radon transform.
- 1963: Allan Cormack publishes mathematical analysis of tomographic image reconstruction, unaware of Radon's work.
- 1972: Godfrey Hounsfield develops first CT system, unaware of either Radon or Cormack's work, develops his own reconstruction method.
- 1979 Hounsfield and Cormack receive the Nobel Prize in Physiology or Medicine.



Radon

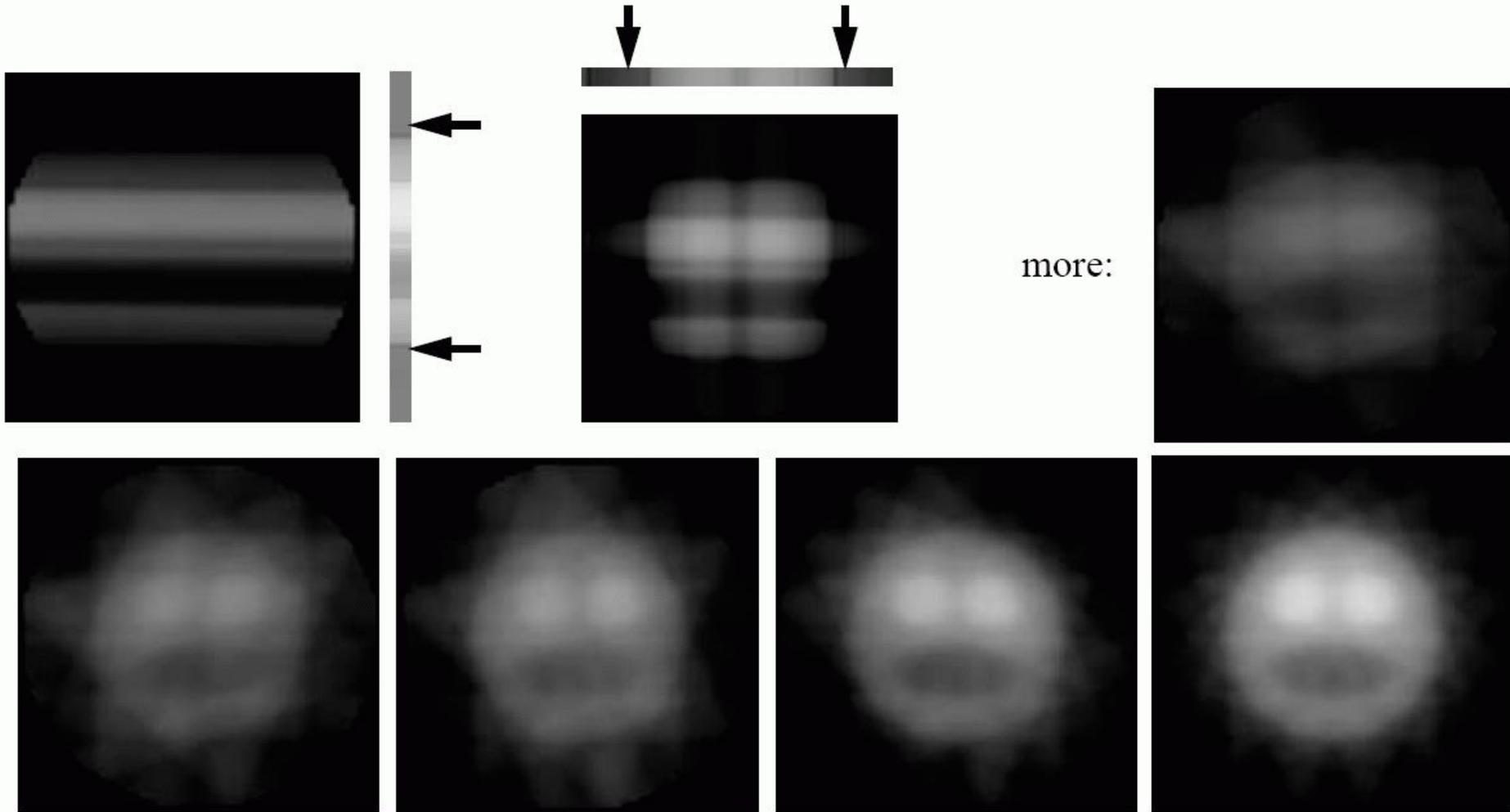


Cormack



Hounsfield

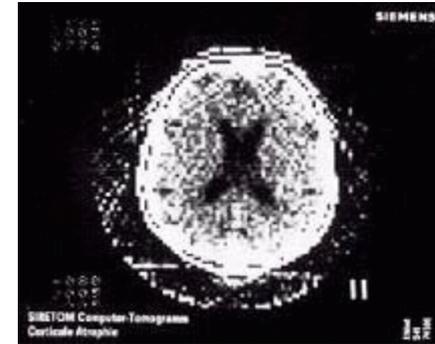
# Computed Tomography: Concept



# Computed Tomography: Past and Present

Image from the Siemens Siretom CT scanner, ca. 1975

- 128x128 matrix.



Modern CT image acquired with a Siemens scanner

- 512x512 matrix



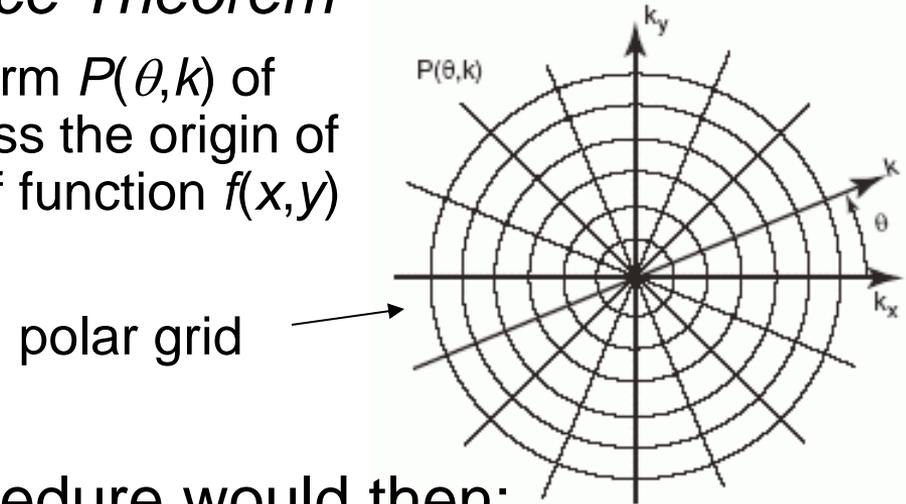
# Slice Viewer



# The Fourier Slice Theorem

To understand the blurring we need more theory → the *Fourier Slice Theorem* or *Central Slice Theorem*

- it states that the Fourier transform  $P(\theta, k)$  of a projection  $p(r, \theta)$  is a line across the origin of the Fourier transform  $F(k_x, k_y)$  of function  $f(x, y)$

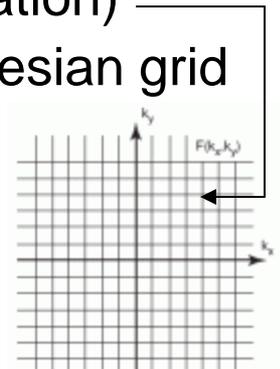


A possible reconstruction procedure would then:

- calculate the 1D FT of all projections  $p(r_m, \theta_m)$ , which gives rise to  $F(k_x, k_y)$  sampled on a polar grid (see figure)
- resample the polar grid into a cartesian grid (using interpolation)
- perform inverse 2D FT to obtain the desired  $f(x, y)$  on a cartesian grid

However, there are two important observations:

- interpolation in the frequency domain leads to artifacts
- at the FT periphery the spectrum is only sparsely sampled



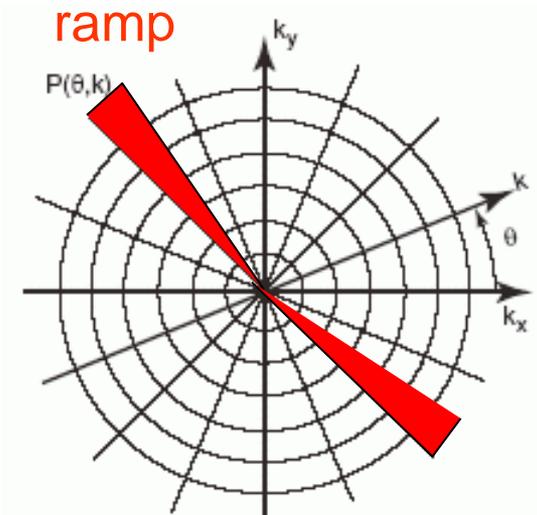
# Filtered Backprojection: Concept

To account for the implications of these two observations, we modify the reconstruction procedure as follows:

- filter the projections to compensate for the blurring
- perform the interpolation in the spatial domain via backprojection  
→ hence the name *Filtered Backprojection*

Filtering -- what follows is a more practical explanation (for formal proof see the book):

- we need a way to equalize the contributions of all frequencies in the FT's polar grid
- this can be done by multiplying each  $P(\theta, k)$  by a ramp function → this way the magnitudes of the existing higher-frequency samples in each projection are scaled up to compensate for their lower amount
- the ramp is the appropriate scaling function since the sample density decreases linearly towards the FT's periphery



# Filtered Backprojection: Equation and Result

1D Fourier transform of  $p(r, \theta)$   
 $\rightarrow P(k, \theta)$

$$f(x, y) = \int_0^{\pi} \left( \int_{-\infty}^{\infty} P(k, \theta) \cdot |k| \cdot e^{i2\pi kr} dk \right) d\theta$$

The equation is annotated with three colored boxes and arrows:

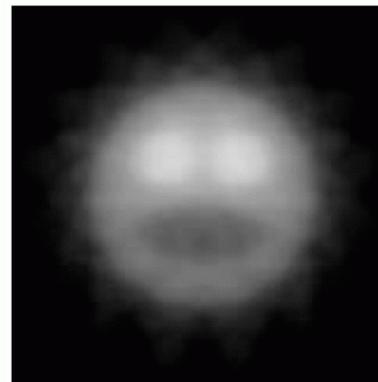
- A red box around the inner integral  $\int_{-\infty}^{\infty} P(k, \theta) \cdot |k| \cdot e^{i2\pi kr} dk$  is labeled "ramp-filtering".
- A green box around the entire expression  $\int_0^{\pi} \left( \int_{-\infty}^{\infty} P(k, \theta) \cdot |k| \cdot e^{i2\pi kr} dk \right) d\theta$  is labeled "inverse 1D Fourier transform  $\rightarrow p(r, \theta)$ ".
- A blue box around the entire equation is labeled "backprojection for all angles".

backprojection for all angles

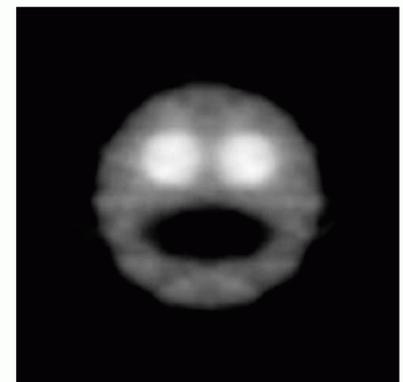
inverse 1D Fourier transform  $\rightarrow p(r, \theta)$

Recall the previous (blurred) backprojection illustration

- now using the filtered projections:



not filtered



filtered

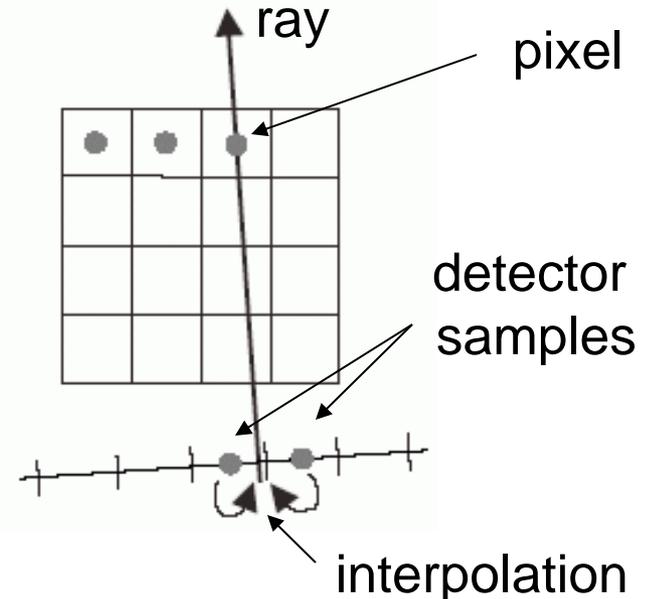
# Backprojection: Practical Considerations

A few issues remain for practical use of this theory:

- we only have a finite set of  $M$  projections and a discrete array of  $N$  pixels  $(x_i, y_j)$

$$b(x_i, y_j) = B\{p(r_n, \theta_n)\} = \sum_{m=1}^M p(x_i \cdot \cos \theta_m + y_j \cdot \sin \theta_m, \theta_m)$$

- to reconstruct a pixel  $(x_i, y_j)$  there may not be a ray  $p(r_n, \theta_n)$  (detector sample) in the projection set  
→ this requires interpolation (usually **linear interpolation** is used)



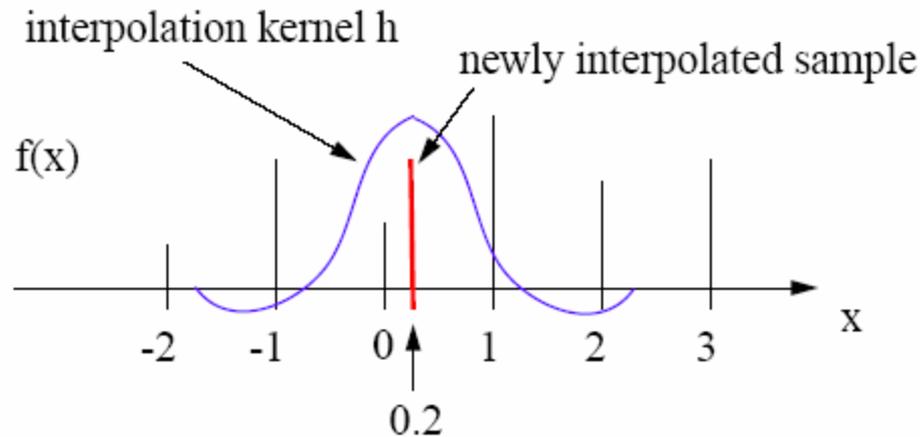
- the reconstructions obtained with the simple backprojection appear blurred (see previous slides)

# Interpolation

Often we want to estimate the formerly continuous function from the discretized function represented by the matrix of sample points

This is done via *interpolation*

Concept:

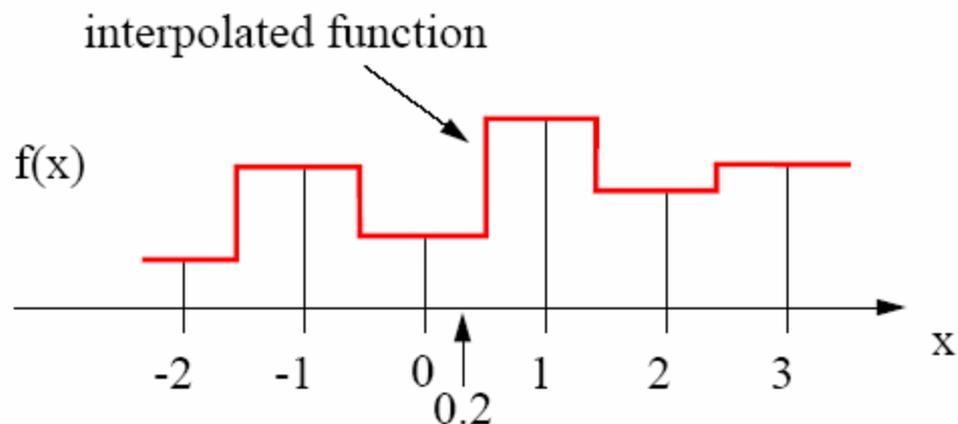
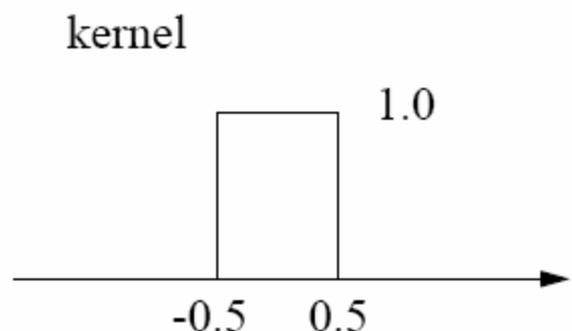


- center the interpolation kernel (filter)  $h$  at the sample position and superimpose it onto the grid
- multiply the values of the grid samples with the kernel value at the superimposed position
- add all the products  $\rightarrow$  this gives the value of the newly interpolated sample
- in the shown case:

$$f(0.2) = h(-0.2) f(0) + h(-1.2) f(-1) + h(0.8) f(1) + h(1.8) f(2)$$

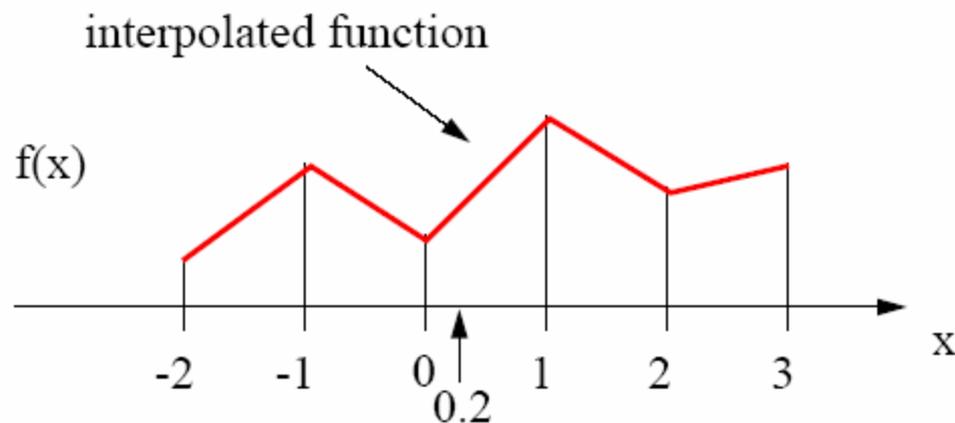
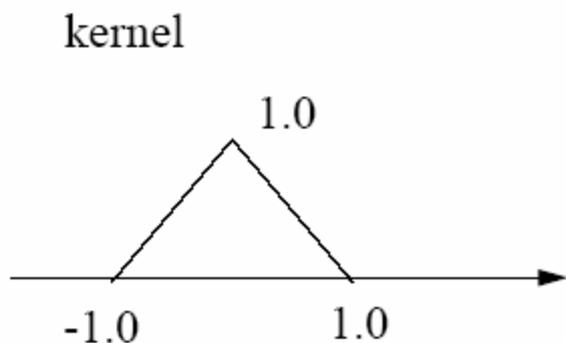
# Interpolation Kernels (1)

- Nearest Neighbor:



- simply pick the value of the nearest grid point:  $f(0.2) = f(\text{trunc}(0.2+0.5)) = f(\text{round}(0.2))$

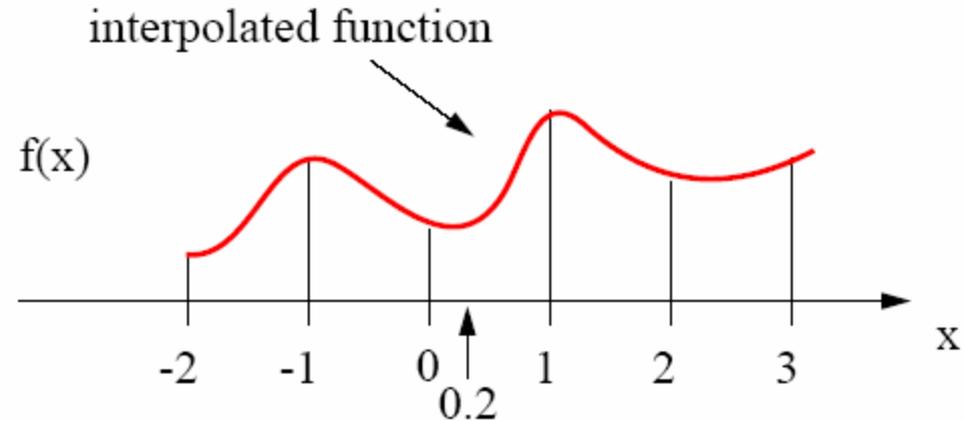
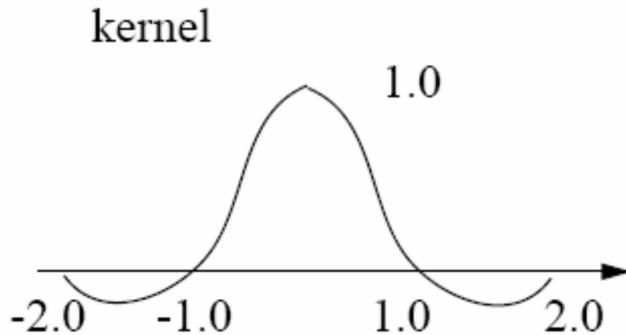
- Linear filter:



- use a linear combination of the two neighboring grid values:  $f(0.2) = 0.2 \cdot f(1) + 0.8 \cdot f(0)$

# Interpolation Kernels (2)

- Cubic filter:



An additional popular filter is the Gaussian function

Discussion:

- nearest neighbor is fastest to compute (just one add), gives sharp edges, but sometimes jagged lines
- linear interpolation takes 2 mults and 1 add and gives a piecewise smooth function
- cubic filter takes 4 mults and 3 adds, but gives an overall smooth interpolated function
- linear interpolation is most popular in many application

# Interpolation in Higher Dimensions

- All interpolation kernels shown here are separable

$$h(x, y) = h(x) \cdot h(y) \quad \text{and} \quad h(x, y, z) = h(x) \cdot h(y) \cdot h(z)$$

- Linear interpolation

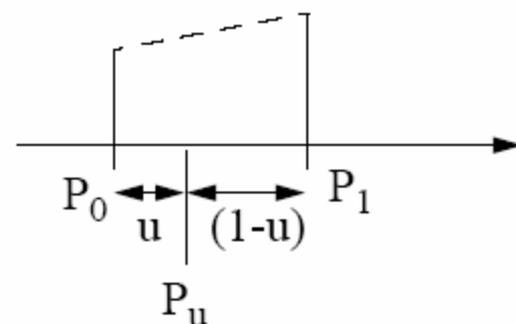
assume: grid distance = 1.0

$P_u$  is the location of the sample value

$P_0$  and  $P_1$  are neighboring grid points

then:  $u = P_u - P_0$

$$f(x) = f(P_u) = (1 - u) \cdot f(P_0) + u \cdot f(P_1)$$



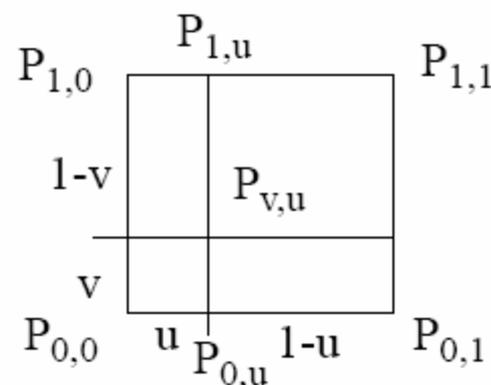
- Bilinear interpolation

$$f(P_{0,u}) = (1 - u) \cdot f(P_{0,0}) + u \cdot f(P_{0,1})$$

$$f(P_{1,u}) = (1 - u) \cdot f(P_{1,0}) + u \cdot f(P_{1,1})$$

$$f(P_{v,u}) = (1 - v) \cdot f(P_{0,u}) + v \cdot f(P_{1,u})$$

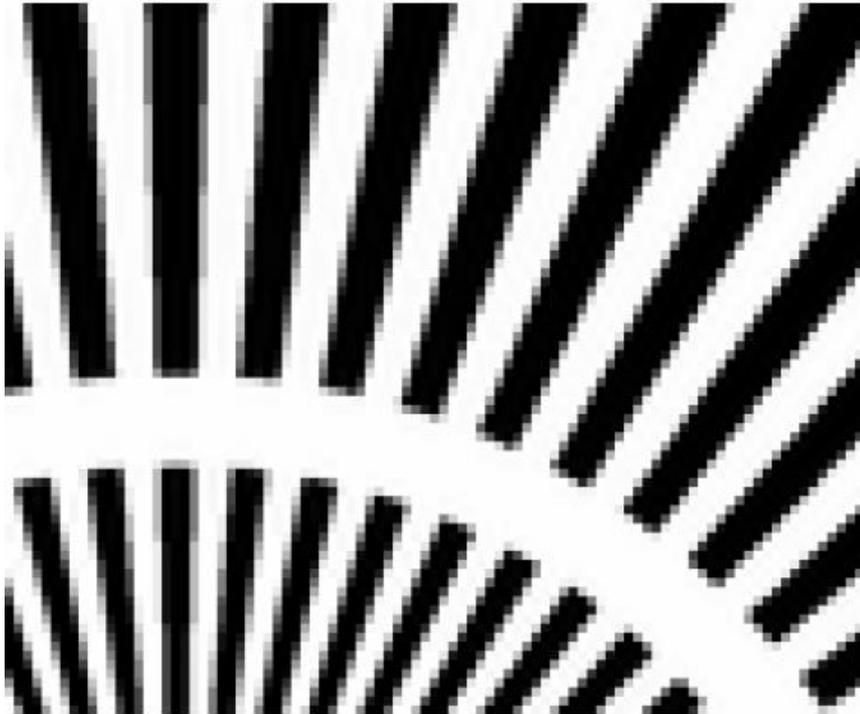
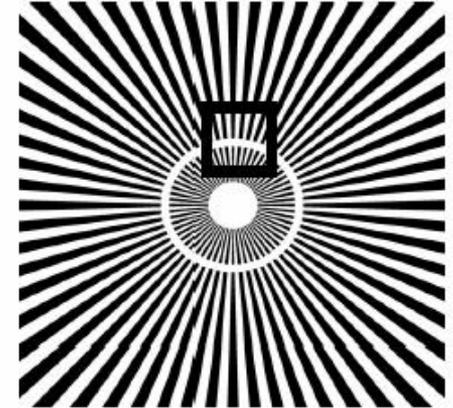
$$\rightarrow f(x, y) = f(P_{v,u}) = (1-v) (1-u) f(P_{0,0}) + (1-v) u f(P_{0,1}) + v (1-u) f(P_{1,0}) + v u f(P_{1,1})$$



# Interpolation Quality

Example:

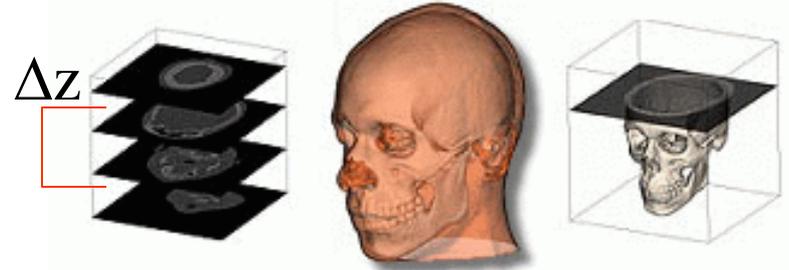
- resampling of a portion of the star image onto a high resolution grid
- magnification factor  $\sim 20$



# Imaging in Three Dimensions: Spiral CT

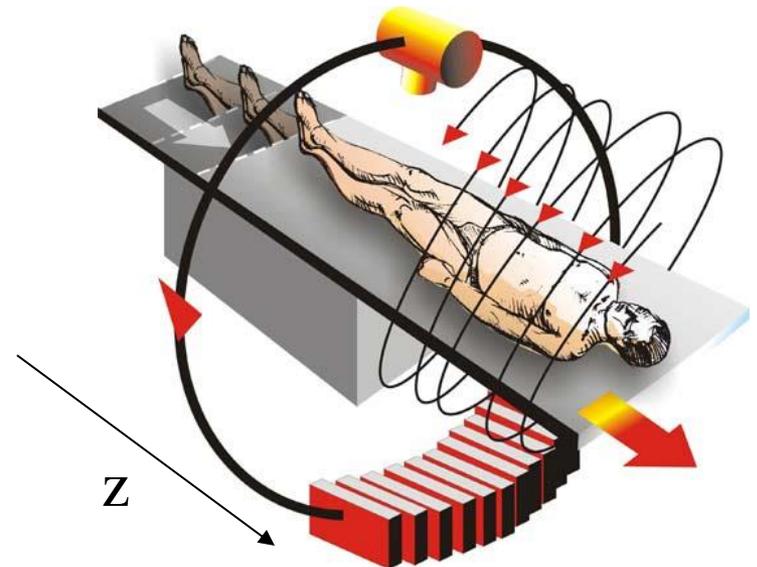
## Sequential CT

- advance table with patient after each slice acquisition has been completed
- stop-motion is time consuming and also shakes the patient
- the *effective thickness* of a slice,  $\Delta z$ , is equivalent to the beam width  $\Delta s$  in 2D
- similarly: we must acquire 2 slices per  $\Delta z$  to combat aliasing



## Spiral (helical) CT

- table translates as tube rotates around the patient
- very popular technique
- fast and continuous
- *table feed (TF)* = axial translation per tube rotation
- *pitch* =  $TF / \Delta z$



# 3D Reconstruction From Cone-Beam Data

## Most direct 3D scanning modality

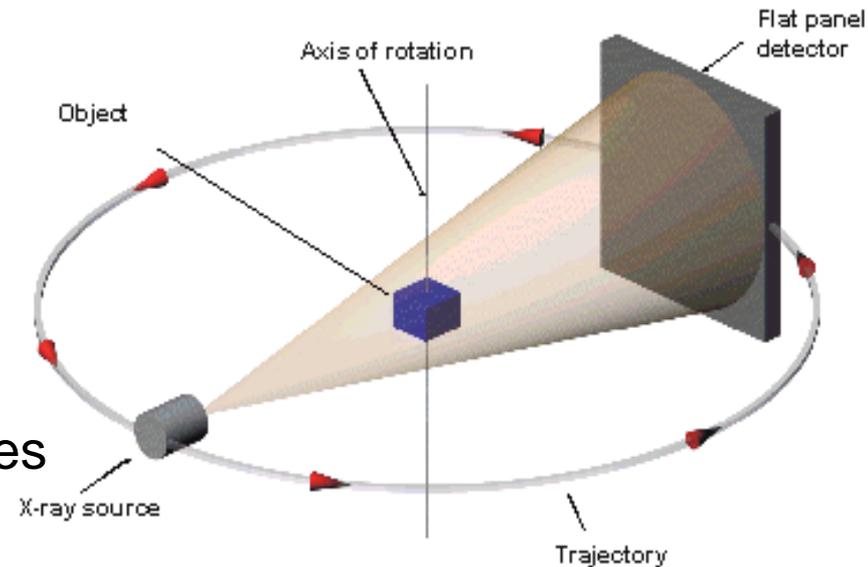
- uses a 2D detector
- requires only one rotation around the patient to obtain all data (within the limits of the cone angle)
- reconstruction formula can be derived in similar ways than the fan beam equation (uses various types of weightings as well)
- a popular equation is that by Feldkamp-Davis-Kress (FDK)
- backprojection proceeds along cone-beam rays

## Advantages

- potentially very fast (since only one rotation)
- often used for 3D angiography

## Downsides

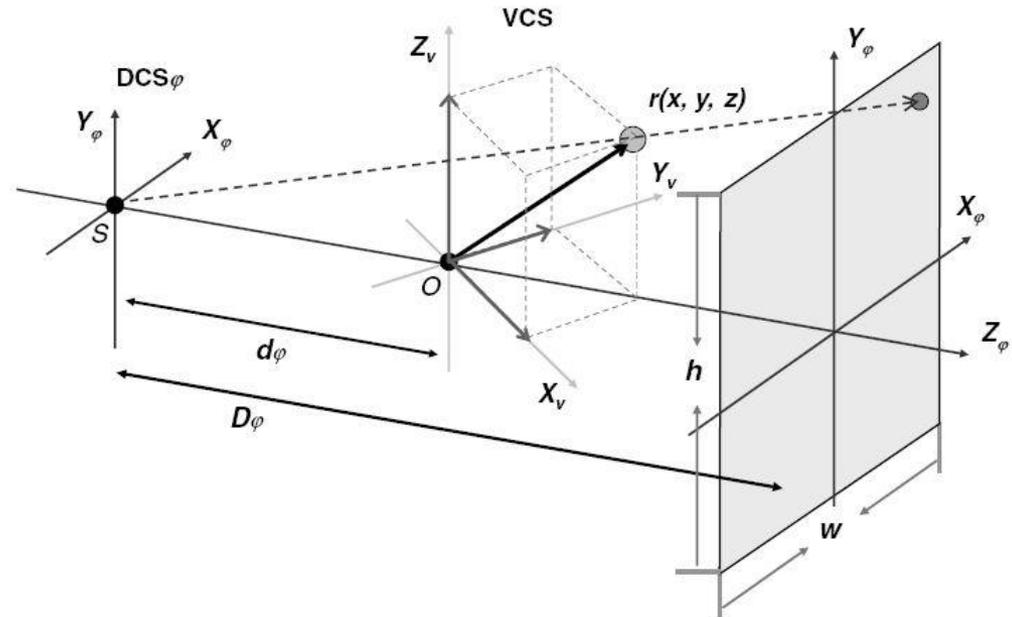
- sampling problems at the extremities
- reconstruction sampling rate varies along z



# Cone-Beam Reconstruction Geometry

Per voxel, for each angle

- determine ray from voxel to source
- intersect with detector plane
- determine detector pixels
- interpolate these
- do depth weighting
- add contribution to voxel



$$v_\phi(\mathbf{r}) = \frac{d_\phi^2}{(d_\phi + \mathbf{r} \cdot \mathbf{z}_\phi)^2} \cdot \text{Int}(P_\phi(X_\phi(\mathbf{r}), Y_\phi(\mathbf{r}))),$$

$$X(\mathbf{r}) = \frac{\mathbf{r} \cdot \mathbf{x}_\phi}{d_\phi + \mathbf{r} \cdot \mathbf{z}_\phi} D_\phi, \quad Y(\mathbf{r}) = \frac{\mathbf{r} \cdot \mathbf{y}_\phi}{d_\phi + \mathbf{r} \cdot \mathbf{z}_\phi} D_\phi.$$

# Rabbit CT

## Benchmarking framework:

- developed By Rohkohl et al.
- FDK backprojection algorithm
- 496 projections of a rabbit
- 1248 X 960 pixels each

## Advantages:

- enables true comparisons
- embeds the system matrix already
- 'just' accelerate the backprojection
- measures timings
- measures reconstruction errors

## Leaderboard

- benchmark new code
- $256^3$ ,  $512^3$ ,  $1024^3$  volume reconstructions



# Rabbit CT Leaderboard (May 14, 2013)

## Ranking

Problem size: [256](#) | **512** | [1024](#)

Rank	Algorithm Description	$q_{rmse}^*$ [HU]	Error Hist.†	PSNR‡ [dB]	Time+ [s]	Performance*
1	 <b>Thumper</b> Submitter: Timo Zinßer Institution: Siemens AG RabbitCT dataset version: 2	0.16		88.30	0.8	<b>100.00%</b>
Thumper is a CUDA-based back-projection implementation.						
2	 <b>CERA on GTX 680</b> Submitter: Matthias Elter Institution: Siemens AG RabbitCT dataset version: 2	0.18		87.38	0.9	<b>87.94%</b>
The CUDA 5.0 based CERA back-projection implementation (extended with CUDA streams) running on a NVIDIA GTX 680.						
3	 <b>RapidRabbit</b> Submitter: Eric Papenhausen, Ziyi Zheng Institution: Stony Brook University RabbitCT dataset version: 1	2.84		63.17	3.0	<b>26.68%</b>
A CUDA 3.0 based back projection implementation using a variety of optimization techniques.						
4	 <b>CERA on GTX 670</b> Submitter: Matthias Elter Institution: Siemens AG RabbitCT dataset version: 1	2.84		63.17	3.4	<b>23.20%</b>
A CUDA 4.2 based back-projection implementation running on a NVIDIA GTX 670 GPU.						
5	 <b>CERA on GTX 570</b> Submitter: Matthias Elter Institution: Siemens AG RabbitCT dataset version: 1					

# Rabbit CT Leaderboard (May 14, 2013)

## Ranking

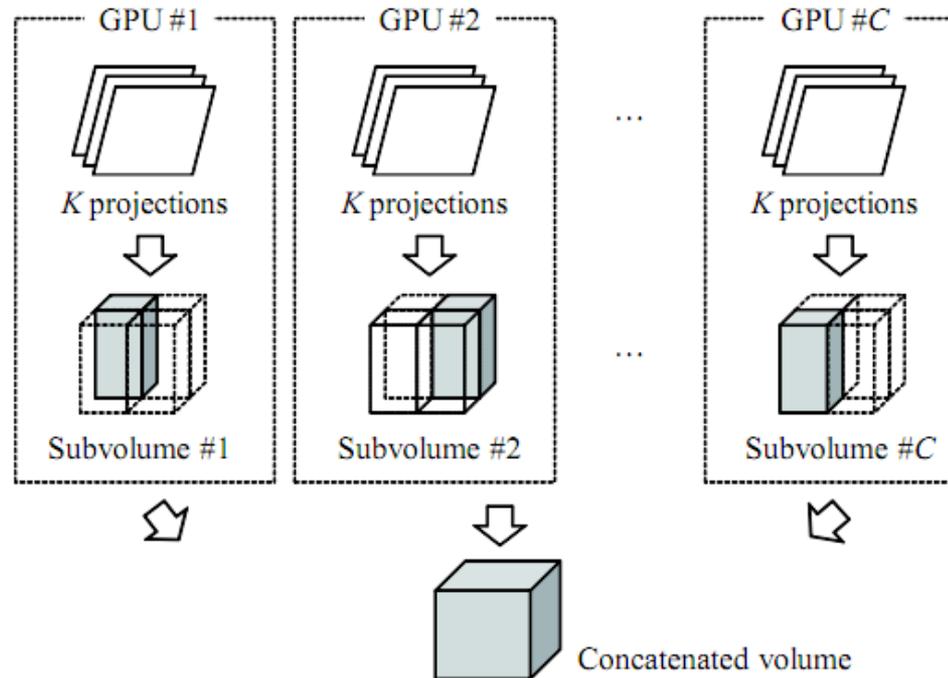
Problem size: [256](#) | **512** | [1024](#)

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<b>5</b>	 <b>CERA on GTX 570</b> Submitter: Matthias Elter Institution: Siemens AG RabbitCT dataset version: 1					

# Rapid Rabbit (June, 2011)

## Approach:

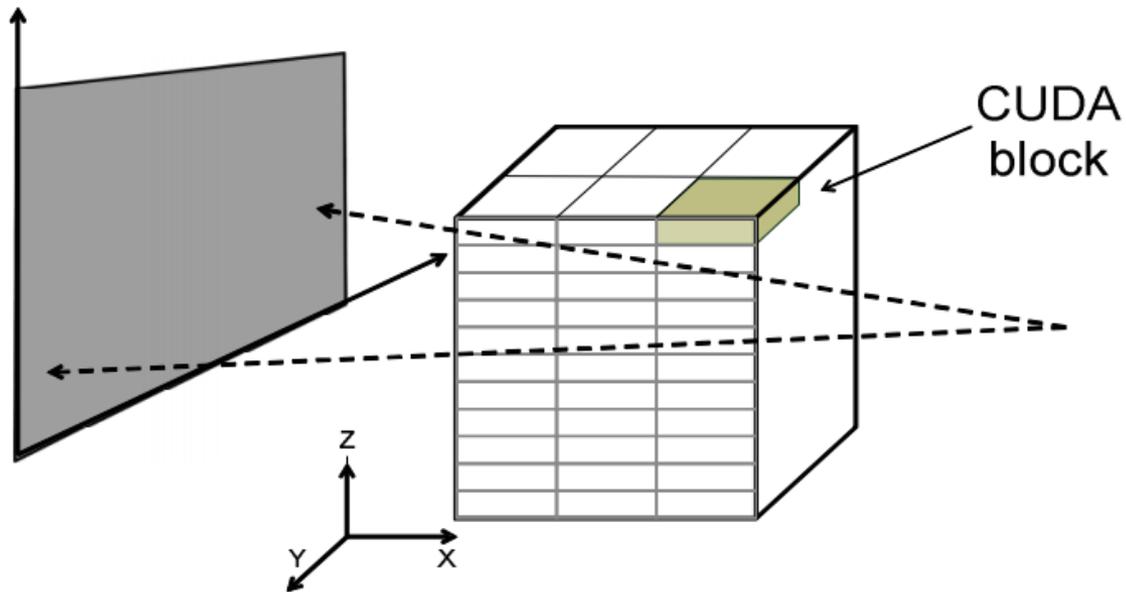
- voxel parallelism
- each thread block computes a subset of the volume



# Setup

Approach:

- each thread computes an array of voxels



Thread Block Dimension:  $16 \times 16 \times 4$

# Naïve Implementation

## Approach:

- volume, projection image, and projection matrix stored in global memory
- explicit bi-linear interpolation

# Naïve Implementation

```
row = blockIdx.y * blockDim.y + threadIdx.y  
col = blockIdx.x * blockDim.x + threadIdx.x
```

```
FOR k = 0 to L
```

```
  x = O_L + col * R_L  
  y = O_L + row * R_L  
  z = O_L + k * R_L
```

```
  w = A[2] * x + A[5] * y + A[8] * z + A[11]  
  u = (A[0] * x + A[3] * y + A[6] * z + A[9]) / w  
  v = (A[1] * x + A[4] * y + A[7] * z + A[10]) / w
```

```
  result = interpolate (u, v)  
  result = result / w2
```

```
  f_L[k * L2 + row * L + col] += result  
END
```

# Naïve Results

256<sup>3</sup>:

- Total: 7.77 s
- Mean: 15.66 ms
- Error: 8.04 HU<sup>2</sup>
- GUPS: 0.99

512<sup>3</sup>:

- Total: 42.6 s
- Mean: 86.06 ms
- Error: 8.04 HU<sup>2</sup>
- GUPS: 1.45

Floating Point to Memory Access Ratio is 4:1  
Explicit Bi-linear interpolation = Low Occupancy

# ASIC

## Approach:

- Projection Image stored in Texture Memory
- Projection Matrix stored in Constant Memory
- ASIC = Fast 2D texture interpolation

# ASIC

```
texture<float, 2> texRef  
__constant__ float A[12]
```

```
row = blockIdx.y * blockDim.y + threadIdx.y  
col = blockIdx.x * blockDim.x + threadIdx.x  
FOR k = 0 to L
```

```
    result = f_L[k * L2 + row * L + col]
```

```
    x = O_L + col * R_L  
    y = O_L + row * R_L  
    z = O_L + k * R_L
```

```
    w = A[2] * x + A[5] * y + A[8] * z + A[11]  
    u = (A[0] * x + A[3] * y + A[6] * z + A[9]) / w  
    v = (A[1] * x + A[4] * y + A[7] * z + A[10]) / w  
    result += tex2D ( texRef, (u + 0.5), (v + 0.5)) / w2
```

```
    f_L[k * L2 + row * L + col] = result  
END
```

# ASIC Results

256<sup>3</sup>:

- Total: 3.53 s
- Mean: 7.13 ms
- Error: 8.07 HU<sup>2</sup>
- GUPS: 2.19

512<sup>3</sup>:

- Total: 10.8 s
- Mean: 21.82 ms
- Error: 8.07 HU<sup>2</sup>
- GUPS: 5.73

Lower bound of 2 global memory accesses

All threads access same constant memory location

ASIC Interpolation = Fewer Registers = Higher Occupancy

# Fully Optimized

## Approach:

- Similar to ASIC, but increased thread granularity
- Each thread operates on same voxels
- 4 projections per kernel invocation

# Fully Optimized

```
texture<float, 2> tRef, tRef2, tRef3, tRef4
```

```
__constant__ float A[48]
```

```
row = blockIdx.y * blockDim.y + threadIdx.y
```

```
col = blockIdx.x * blockDim.x + threadIdx.x
```

```
FOR k = 0 to L
```

```
    result = f_L[k * L2 + row * L + col]
```

```
    ...
```

```
    // mapping voxel (x,y,z) to projection 1 and backproject
```

```
    w = A[2] * x + A[5] * y + A[8] * z + A[11]
```

```
    u = (A[0] * x + A[3] * y + A[6] * z + A[9]) / w
```

```
    v = (A[1] * x + A[4] * y + A[7] * z + A[10]) / w
```

```
    result += tex2D ( tRef, (u + 0.5), (v + 0.5)) / w2
```

```
    //repeat for projection 2 with A[12-23] and tRef2
```

```
    //repeat for projection 3 with A[24-35] and tRef3
```

```
    // repeat for projection 4 with A[36-47] and tRef4
```

```
    f_L[k * L2 + row * L + col] = result
```

```
END
```

# Fully Optimized Results

256<sup>3</sup>:

- Total: 2.71 s
- Mean: 5.47 ms
- Error: 8.07 HU<sup>2</sup>
- GUPS: 2.86

512<sup>3</sup>:

- Total: 6.07 s
- Mean: 12.25 ms
- Error: 8.07 HU<sup>2</sup>
- GUPS: 10.2

Still Lower bound of 2 global memory accesses per iteration

Overall memory accesses decreased by a factor of 4

Greater than 4 projections led to degraded performance

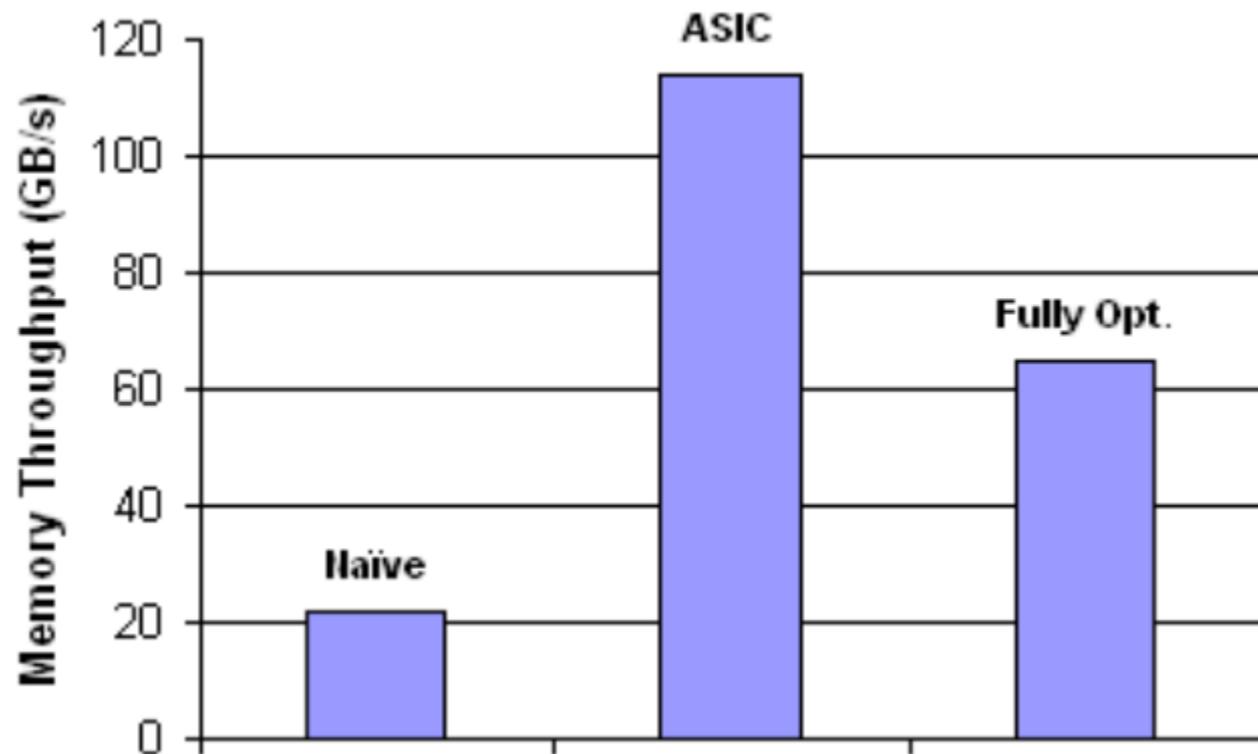
# Results

Configuration	Volume	Total	Mean	Error	Speed-up	GUPS
Naïve	$256^3$	7.77s	15.66ms	8.04HU <sup>2</sup>	N/A	0.99
ASIC	$256^3$	3.53s	7.13ms	8.07HU <sup>2</sup>	2.19	2.19
Fully Opt.	$256^3$	2.71s	5.47ms	8.07HU <sup>2</sup>	1.3	2.86
Naïve	$512^3$	42.6s	86.08ms	8.04HU <sup>2</sup>	N/A	1.45
ASIC	$512^3$	10.8s	21.82ms	8.07HU <sup>2</sup>	3.9	5.73
Fully Opt.	$512^3$	6.07s	12.25ms	8.07HU <sup>2</sup>	1.78	10.2

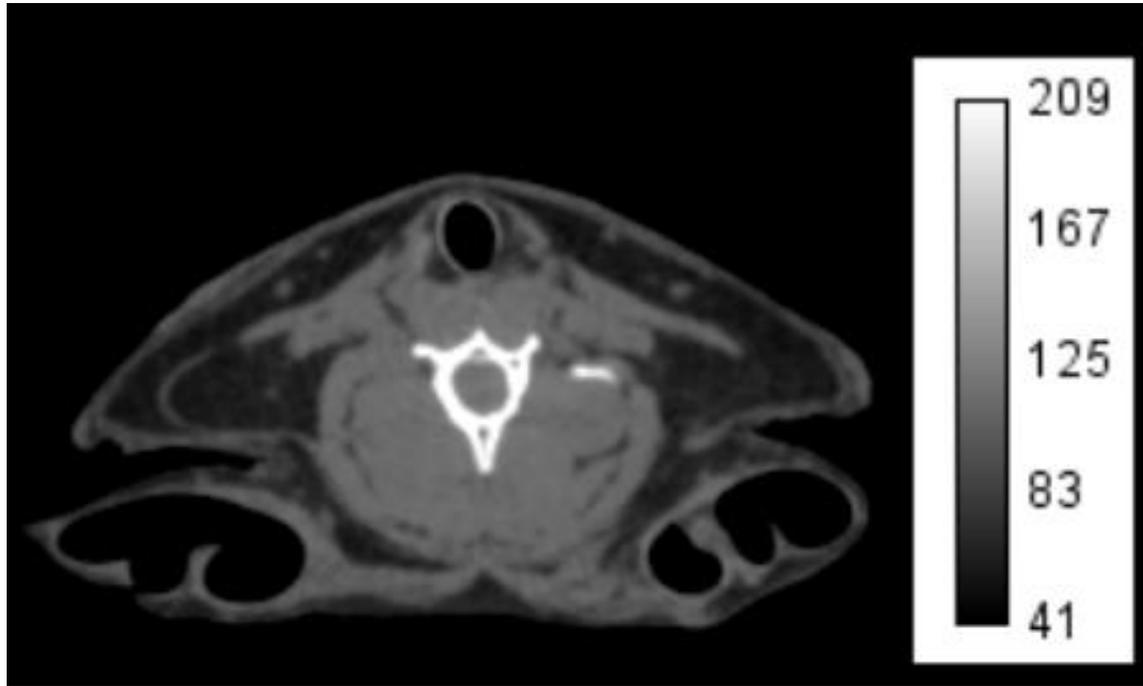
# Results

Configuration	Volume	Total	Mean	Error	Speed-up
Best Known	256 <sup>3</sup>	3.843s	7.75ms	8.07HU <sup>2</sup>	N/A
Fully Opt.	256 <sup>3</sup>	2.713s	5.47ms	8.07HU <sup>2</sup>	1.4
Best Known	512 <sup>3</sup>	13.94s	28.11ms	8.07HU <sup>2</sup>	N/A
Fully Opt.	512 <sup>3</sup>	6.076s	12.25ms	8.07HU <sup>2</sup>	2.29

# Results



# Results



Click for more [paper](#)

Eric Papenhausen, Ziyi Zheng, and Klaus Mueller. "GPU-accelerated back-projection revisited: squeezing performance by careful tuning." Workshop on High Performance Image Reconstruction (HPIR). 2011.

# Optimizations

## Successful:

- Pre-fetching
- Page-locked memory

## Unsuccessful:

- Loop Unrolling
- Fast Math

Common Sense Optimizations

# New Rabbit on the Block: Thumper (March 2013)

Improves upon Rapid Rabbit

Initial code (kernel A)

---

```
compute position of first voxel
for  $I$  input projections do
  | compute homogeneous detector coordinates  $q[i]$  of first voxel
end
for  $K$  consecutive voxels along the  $z$ -axis do
  | zero-initialize sum  $s$  of weighted back-projected values
  | for  $I$  input projections do
  |   | dehomogenize detector coordinates  $q[i]$ 
  |   | compute back-projected value by texture fetching
  |   | update sum  $s$  of weighted back-projected values
  |   | update homogeneous detector coordinates  $q[i]$ 
  | end
  | update volume at current voxel with computed sum  $s$ 
  | (optionally) synchronize threads in thread block
end
```

---

Click for more [info](#) and [paper](#)

Timo Zinsser, and Benjamin Keck. "Systematic performance optimization of cone-beam back-projection on the Kepler architecture." Proceedings of the 12th Fully Three-Dimensional Image Reconstruction in Radiology and Nuclear Medicine (2013): 225-228.

# Analyze Bottlenecks

## Step 1:

- reduce the voxel size from 0.5 mm to  $10^{-6}$  mm
- as a result, all computed detector coordinates are virtually identical
- the hit rate of the texture cache rises to almost one hundred percent

## Step 2:

- disable the texture fetching completely

## Step 3:

- turn off the volume update
- this removes all memory accesses
- leaves only the arithmetic and control flow instructions

## Caution

- do not allow the compiler to eliminate more code than intended
- these modifications also tend to reduce the register count
- so allocate a suitable amount of shared memory to retain the occupancy of the original kernel

# Analyze Bottlenecks

In table:

- I(nstruction), M(emory), T(exture)

Test	Kernel	Sync	$I$	$K$	$B_x$	$B_y$	Occupancy	I - -	I M -	I M T	Time	GUPS
1	A	no	1	512	32	8	1.000	1091 ms	4710 ms	4707 ms	9141 ms	7.3
2	A	no	4	512	32	8	0.750	575 ms	1199 ms	1196 ms	7802 ms	8.5
3	A	yes	4	512	32	8	1.000	554 ms	1185 ms	1169 ms	2710 ms	24.6
4	A	no	4	8	32	8	0.750	685 ms	980 ms	1085 ms	1990 ms	33.4

Test 1:

- kernel A processes one projection at a time
- specified tile width  $B_x = 32$  ensures that the volume updates are performed by fully coalesced memory transactions
- we see that the memory transfer takes much longer than the computation of the arithmetic instructions (I- vs. IM-)
- time is almost doubled by the cache misses of the texture fetching (IMT vs. Time)

# Analyze Bottlenecks

In table:

- I(nstruction), M(emory), T(exture)

Test	Kernel	Sync	$I$	$K$	$B_x$	$B_y$	Occupancy	I   -   -	I   M   -	I   M   T	Time	GUPS
1	A	no	1	512	32	8	1.000	1091 ms	4710 ms	4707 ms	9141 ms	7.3
2	A	no	4	512	32	8	0.750	575 ms	1199 ms	1196 ms	7802 ms	8.5
3	A	yes	4	512	32	8	1.000	554 ms	1185 ms	1169 ms	2710 ms	24.6
4	A	no	4	8	32	8	0.750	685 ms	980 ms	1085 ms	1990 ms	33.4

Test 2:

- when we process four projections in one kernel, the memory transfer size is reduced considerably (IM-)
- the compute-only kernel also runs much faster, because the number of integer-based index computations is minimized as well (I--)
- however, the time penalty induced by the cache misses of the texture fetching remains very high(IMT vs. Time)

# Analyze Bottlenecks

In table:

- I(nstruction), M(emory), T(exture)

Test	Kernel	Sync	$I$	$K$	$B_x$	$B_y$	Occupancy	I - -	I M -	I M T	Time	GUPS
1	A	no	1	512	32	8	1.000	1091 ms	4710 ms	4707 ms	9141 ms	7.3
2	A	no	4	512	32	8	0.750	575 ms	1199 ms	1196 ms	7802 ms	8.5
3	A	yes	4	512	32	8	1.000	554 ms	1185 ms	1169 ms	2710 ms	24.6
4	A	no	4	8	32	8	0.750	685 ms	980 ms	1085 ms	1990 ms	33.4

Test 3:

- we activate the optional synchronization
- this prevents the divergence of the threads in one thread block with respect to the loop over the voxels along the z-axis
- as a result, the texture fetching is accelerated considerably and the computation time is reduced by about 65% (IMT vs. Time)
- the configuration results in a total of 16 waves of thread blocks, which iterate through the volume along the z-axis one after another.

# Analyze Bottlenecks

In table:

- I(nstruction), M(emory), T(exture)

Test	Kernel	Sync	<i>I</i>	<i>K</i>	<i>B<sub>x</sub></i>	<i>B<sub>y</sub></i>	Occupancy	I - -	I M -	I M T	Time	GUPS
1	A	no	1	512	32	8	1.000	1091 ms	4710 ms	4707 ms	9141 ms	7.3
2	A	no	4	512	32	8	0.750	575 ms	1199 ms	1196 ms	7802 ms	8.5
3	A	yes	4	512	32	8	1.000	554 ms	1185 ms	1169 ms	2710 ms	24.6
4	A	no	4	8	32	8	0.750	685 ms	980 ms	1085 ms	1990 ms	33.4

Test 4:

- a kernel processes only 8 voxels
- this relocates the large scale movement along the z-axis from the loop inside the kernel to the third dimension of the grid of thread blocks
- this improves the hit rate of the texture cache even more
- yields the lowest time

# Reordering The Loop

## Observations

- the cache misses of the texture fetching constitute the major performance bottleneck
- the corresponding textures continuously contend for the limited amount of cache memory
- the memory transfers for the volume update take longer than the computations
- could alleviate the latter by having more projections but this would be bad for the former

## Solution

- reverse the nested loop order

# Reordering The Loop

---

```
compute position of first voxel
for  $K$  consecutive voxels along the  $z$ -axis do
  | zero-initialize sum  $s[k]$  of weighted back-projected values
end
for  $I$  input projections do
  | compute homogeneous detector coordinates  $q$  of first voxel
  | for  $K$  consecutive voxels along the  $z$ -axis do
  | | dehomogenize detector coordinates  $q$ 
  | | compute back-projected value by texture fetching
  | | update sum  $s[k]$  of weighted back-projected values
  | | update homogeneous detector coordinates  $q$ 
  | end
end
for  $K$  consecutive voxels along the  $z$ -axis do
  | update volume at current voxel with computed sum  $s[k]$ 
end
```

---

# Results

## Kernel B

Test	Kernel	Sync	$I$	$K$	$B_x$	$B_y$	Occupancy	I   -   -	I   M   -	I   M   T	Time	GUPS
1	A	no	1	512	32	8	1.000	1091 ms	4710 ms	4707 ms	9141 ms	7.3
2	A	no	4	512	32	8	0.750	575 ms	1199 ms	1196 ms	7802 ms	8.5
3	A	yes	4	512	32	8	1.000	554 ms	1185 ms	1169 ms	2710 ms	24.6
4	A	no	4	8	32	8	0.750	685 ms	980 ms	1085 ms	1990 ms	33.4
5	B	—	4	8	32	8	0.875	542 ms	989 ms	1179 ms	1527 ms	43.6
6	B	—	8	4	16	16	0.750	528 ms	725 ms	966 ms	1296 ms	51.4
7	B	—	16	4	16	32	0.750	506 ms	550 ms	826 ms	1051 ms	63.4
8	B	—	32	4	16	32	0.750	489 ms	494 ms	756 ms	969 ms	68.7

## Test 5:

- replace kernel A with kernel B, but keep all other parameters identical. We clearly observe an improved hit rate of the texture cache.

## Following three tests:

- we increase the number of projections  $I$  and tune the other parameters to obtain minimal computation times

# Data Transfer Optimizations

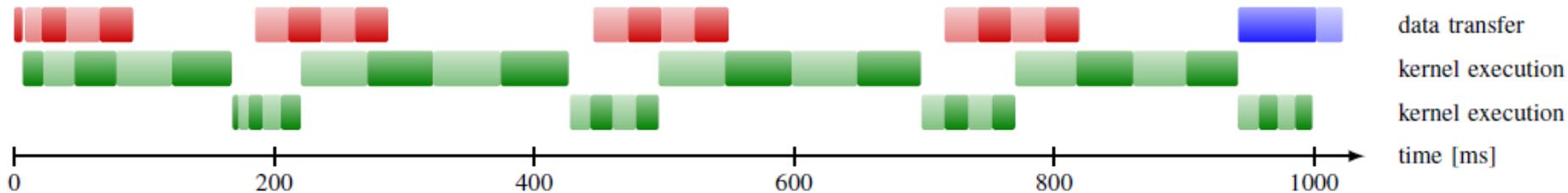
## Transfer requirements

- the  $512^3$  volume results into 2,779 MB of data
- takes about half a second on the system.
- use the ability of our GPU to overlap kernel execution and data transfer to hide this latency
- use CUDA asynchronous kernel launches and asynchronous memcpy functions

# Data Transfer Optimizations

## Strategy

- add 8 projections in each transfer until reaching optimum of 32
- divide volume into two parts (384 and 128 xy slices, resp.)
- gives rise to two kernel executions
- this makes it possible to overlap the download of the first part of the volume with the reconstruction of the second part of the volume



# Results

Volume	Implementation	Type	RMSE	Time	GUPS
512 <sup>3</sup>	fastrabbitEX [4]	CPU	—	7.45 s	8.94
	RapidRabbit [7]	GPU	—	2.98 s	22.3
	Thumper [this work]	GPU	0.021 HU	0.99 s	67.7
1024 <sup>3</sup>	fastrabbitEX [4]	CPU	—	43.8 s	12.2
	CERA [-]	GPU	—	36.1 s	14.7
	Thumper [this work]	GPU	0.021 HU	6.04 s	88.2



# Rapid Rabbit Strikes Back (June 2013)

Inherits insight from Thumper plus additional tricks

Faster perspective divide

- original code

$$w = a_2x + a_5y + a_8z + a_{11}$$

$$u = (a_0x + a_3y + a_6z + a_9) / w$$

$$v = (a_1x + a_4y + a_7z + a_{10}) / w$$

- using fast inverse square root

$$w = a_2x + a_5y + a_8z + a_{11}$$

$$w' = \text{rsqrt}(w * w)$$

$$u = (a_0x + a_3y + a_6z + a_9) * w'$$

$$v = (a_1x + a_4y + a_7z + a_{10}) * w'$$

$$\text{result} += \text{tex2D}(t\text{Ref}, (u+0.5), (v+0.5) * w' * w')$$

Click for more [info](#) and [paper](#)

Eric Papenhausen, Klaus Mueller. "Rapid rabbit: Highly optimized GPU accelerated cone-beam CT reconstruction." IEEE Nuclear Science Symposium and Medical Imaging Conference (NSS/MIC), 2013.

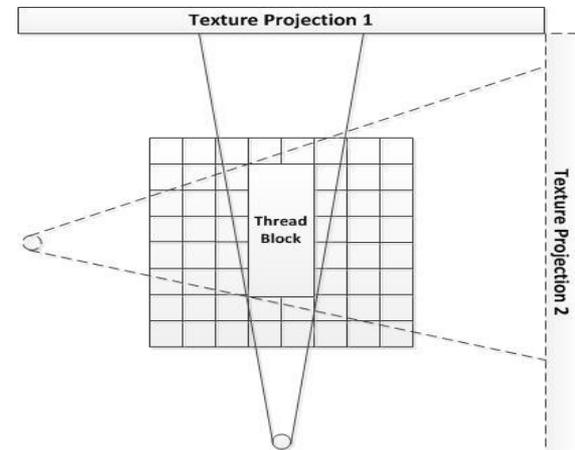
# Rapid Rabbit Strikes Back

## Observation:

- noticed a performance dip between the third and eighth kernel execution
- each kernel execution would last approximately 50 milliseconds at the beginning
- then the kernel executions would gradually get slower until it reached around 65 milliseconds, and then get faster toward the end.
- this dip in performance was because the cache locality was worse in the middle than at the beginning and end of the execution

## Fix:

- transpose the volume at  $45^\circ$
- simply swap x and y indexes



# Rapid Rabbit Strikes Back

## Observation:

- we thought atomic operations were slow
- but with the Kepler architecture, atomics are implemented in an ASIC
- furthermore, atomic operations are executed asynchronously with the calling thread

## How to take advantage:

- accumulate the results into the volume using atomics
- we know that this will be a fast operation since there are no read/write collisions between threads
- thus the asynchronous nature of atomics guarantees that each thread will not have to stall after a write to global memory

# Rapid Rabbit Strikes Back

## Observations:

- in order for us to take advantage of CUDA streams, we have to page-lock the projection memory
- page-locked memory, however, is a scarce resource
- we cannot simply page-lock all the projections at the beginning

## What to do:

- backproject 64 projections before loading another 64 projections into the page-locked memory
- performing the memory copy in another thread to hide some latency
- use ping pong scheme
- one buffer is used for back projection
- the other is copied to switch the buffers

# Rapid Rabbit: Results

Implementation	Thumper	Baseline	+RSQRT	+Transpose	+Multi-Threaded	+Atomics
Timing	0.993 s	2.2 s	1.01s	0.967 s	0.951 s	0.921 s
GUPS	67.7	30.3	65.9	68.8	70.2	72.3

# The Saga Continues...

Come, join the rabbit race

Be the fastest rabbit on the block!

