Introduction to Medical Imaging

Image Operations

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Motivation

Provide the clinician with some means to:

- enhance contrast of local features
- remove noise and other artifacts
- enhance edges and boundaries
- composite multiple images for a more comprehensive view

There are two basic operations: global and local

Global operations:

- operate on the entire set of pixels at once
- examples: brightness and contrast enhancement

Local operations:

- operate only on a subset of pixels (in a pixel neighborhood)
- examples: edge detection, contouring, image sharpening, blurring

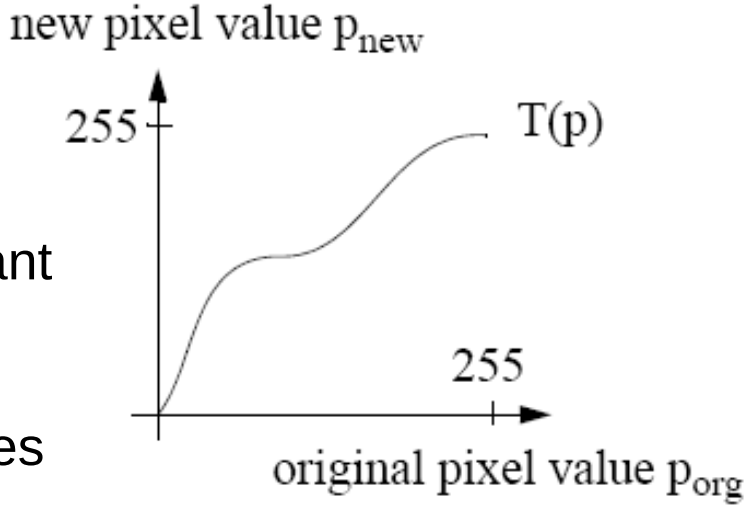
Grey Level Transformation: Basics

We only have a fixed number of grey levels that can be displayed or perceived

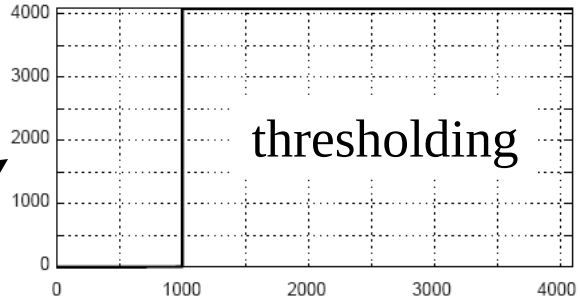
- need to use this ‘real estate’ wisely to bring out the image features that we want

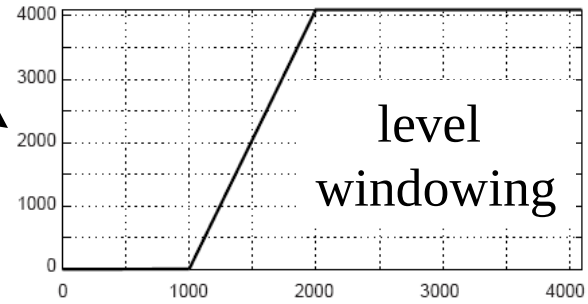
Use *intensity transformations* T_p

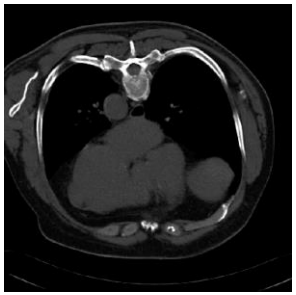
- enhance (remap) certain intensity ranges at the cost of compressing others



lung CT



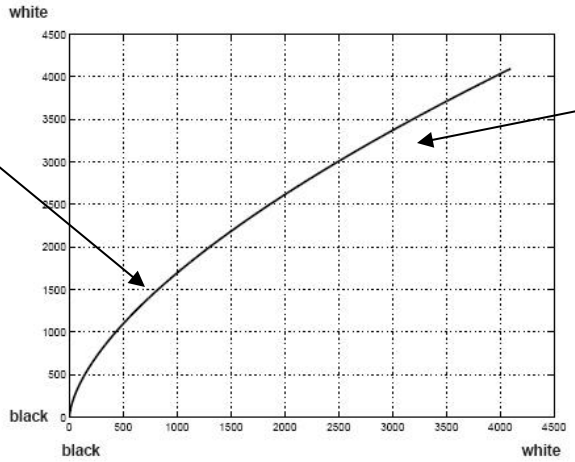




Grey Level Transformation: Enhancements

enhance the dark areas
(slope > 1)

suppress the white areas
(slope < 1)



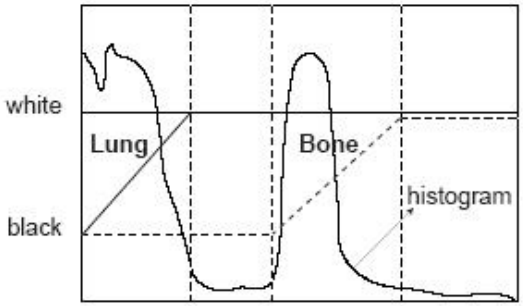
original

enhanced

Grey Level Transformation: Windowing

Dedicate full contrast
to either bone or lungs

original lung
CT image



bi-modal
histogram

bone window

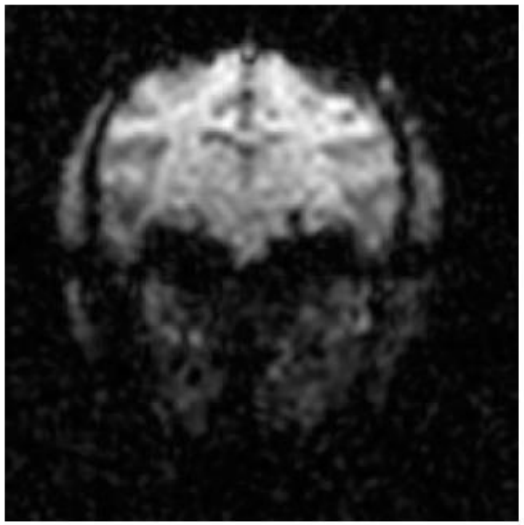
lung window

Multi-Image Operations: Noise Averaging

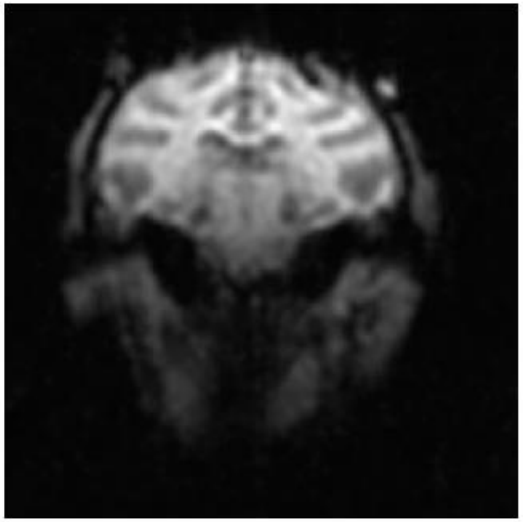
Assume a pixel value *p* is given by: *p = signal + noise*

- E(*signal*) = *signal*
- E(*noise*) = 0, when noise is random

Thus, averaging (adding) multiple images of a steady noisy object will eliminate, or at least reduce, the noise



original



after averaging 16 subsequently acquired images

Multi-Image Operations: Eliminating Background

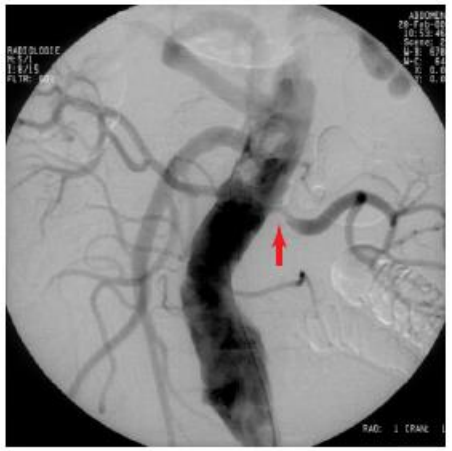
In angiography, radio-opaque contrast agents (injected into the bloodstream) are used to enhance the perfused vessels

An X-ray image is taken when the radio-opaque bolus of blood is coming through

- however, the background reduces the contrast of the dye
- subtracting the (constant) background from the (dynamic) radiographic image leaves just the perfused structures (angio image)

after injection
(radio-image)

background
(mask image)



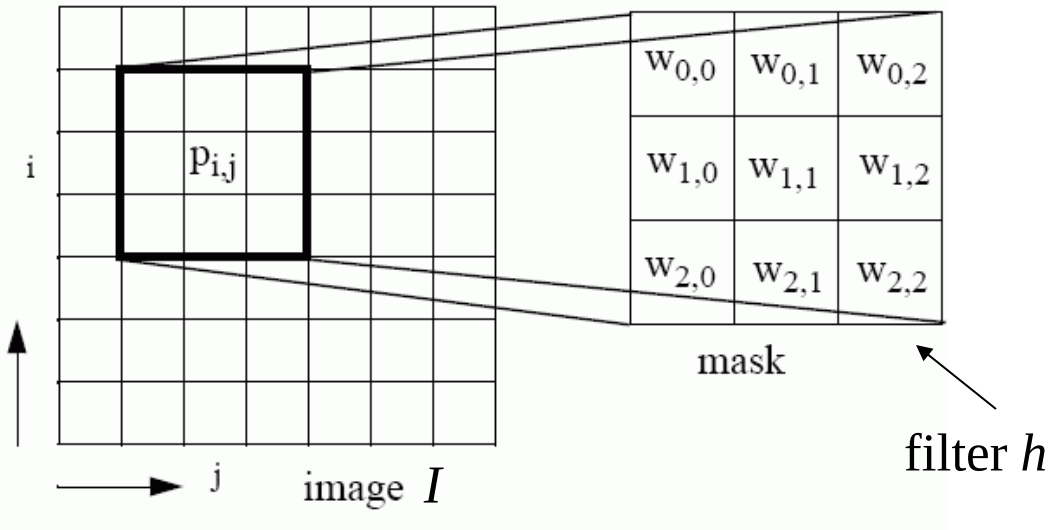
just the bolus
(angio image)

Discrete Filters

We say *discrete filters* since they operate on a discretized signal, the image

- to implement discrete filters we use discrete convolution

$h * I$



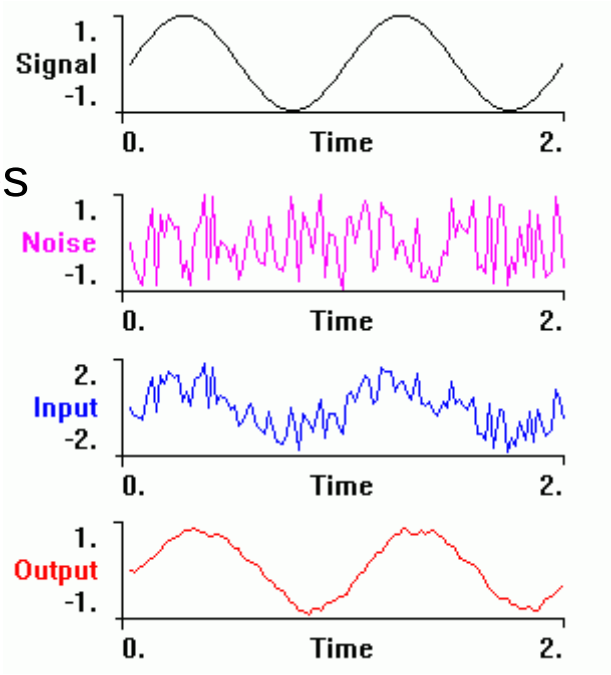
Procedure:

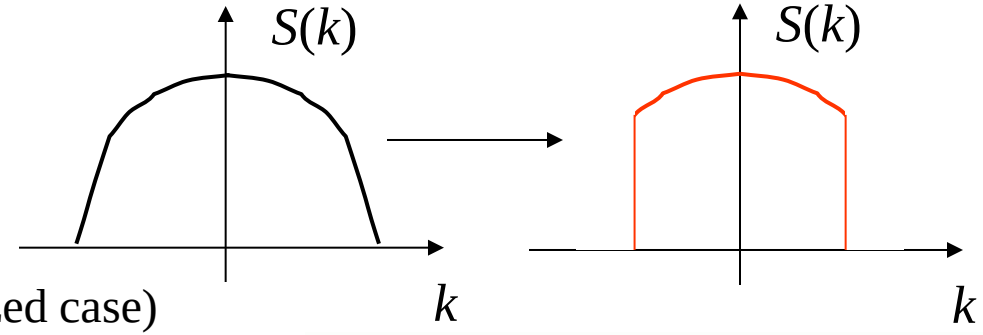
- place a weight matrix or *mask* at each pixel location p_{ij}
- this mask weighs the pixel's neighborhood and determines the output pixel's value
- important: do not replace the computed values into the original image, but write to an output image

Popular Discrete Filters: Lowpass

Smoothing (averaging):

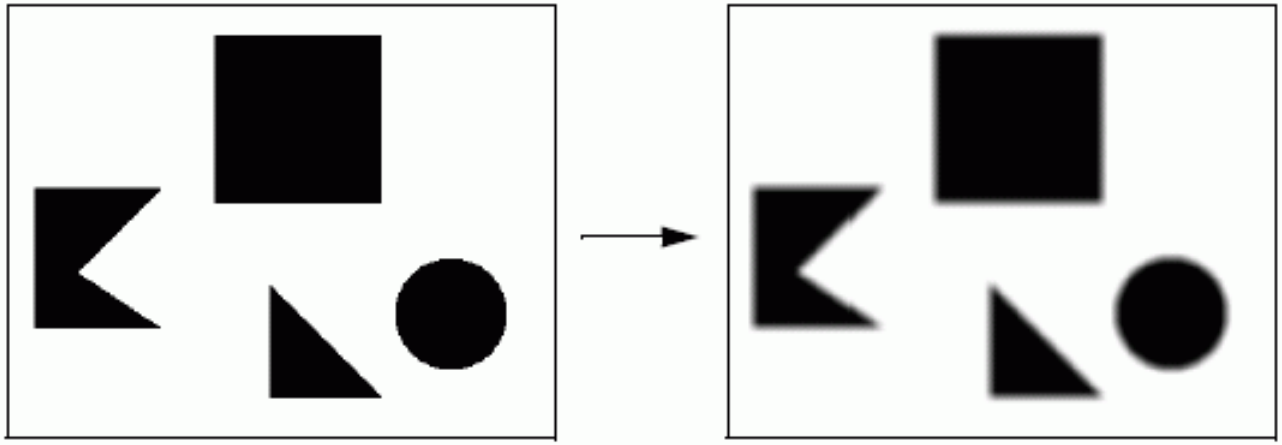
- also called *low-passing:* keeps the low frequencies, but reduces the high frequencies
- removes noise and jagged edges
- but also blurs the signal





(idealized case)

$$1/9 \times \begin{bmatrix} 1 & 1 & 1 \\ 1 & 1 & 1 \\ 1 & 1 & 1 \end{bmatrix}$$



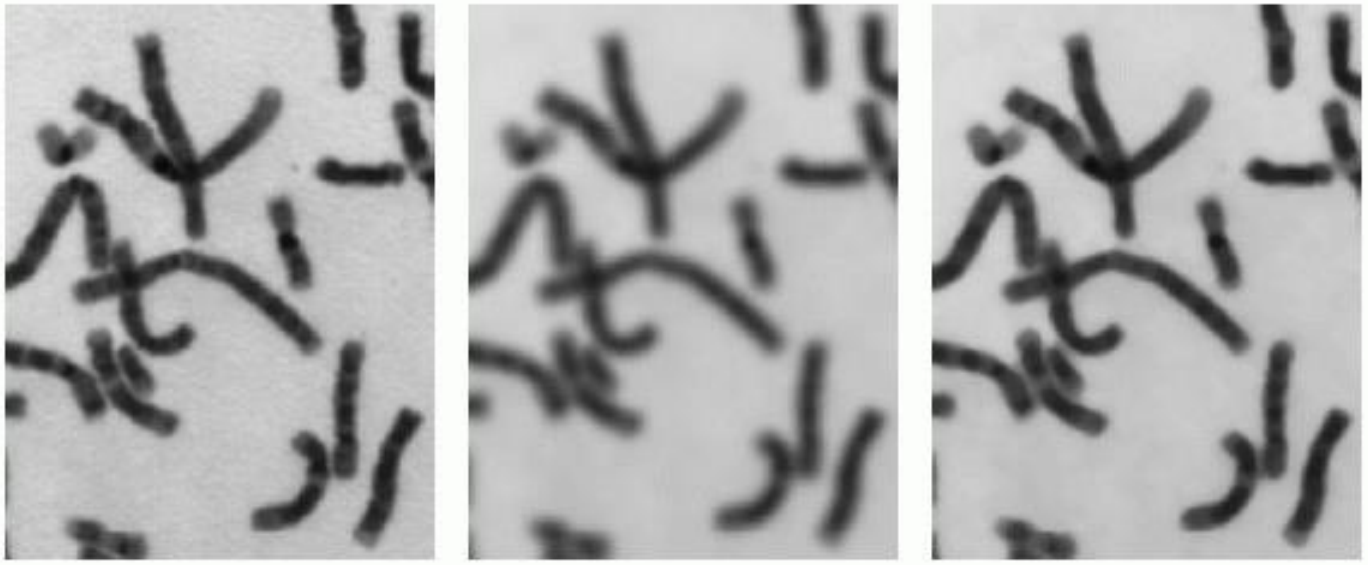
Popular Discrete Filters: Median Smoothing

A non-linear filter, best used to remove speckle noise

- a regular smoothing filter would blur the speckles (and the signal)
- the median filter will elimate the speckle and leave the signal as is

Procedure:

- convolve with a mask as usual
- but this time, for each mask position, sort the values under the mask
- pick the median and write to the output image
- the speckle pixel will be an outlier and not be selected as the median



original smoothed median filtered

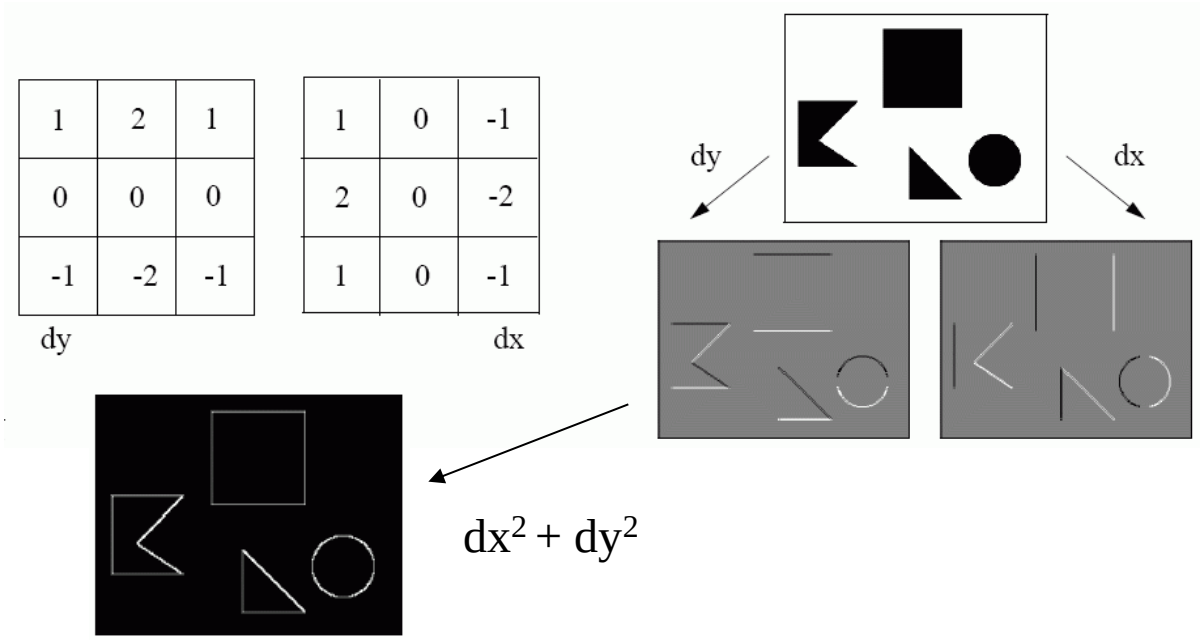
Popular Discrete Filters: Highpass

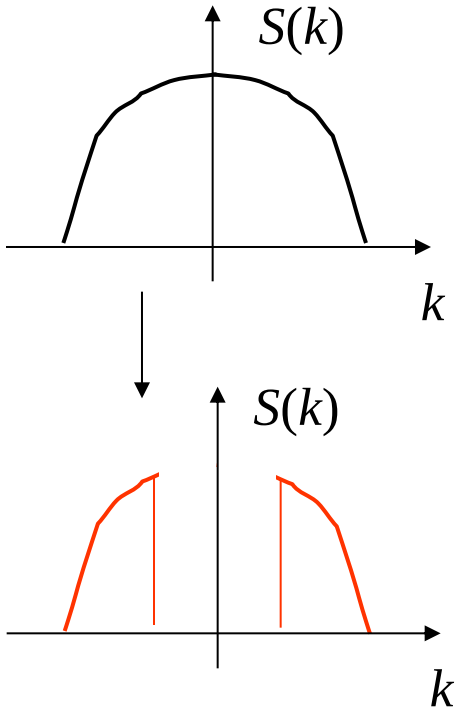
Edge detector / enhancer:

$$\nabla I = \nabla h * I \qquad \text{first derivative (gradient)}$$

$$\nabla^2 I = \nabla^2 h * I \qquad \text{second derivative (Laplacian)}$$

- also called *high-passing:* keeps the high frequencies, but reduces the low frequencies
- enhances edges and contrast
- but also enhances noise and jagged edges





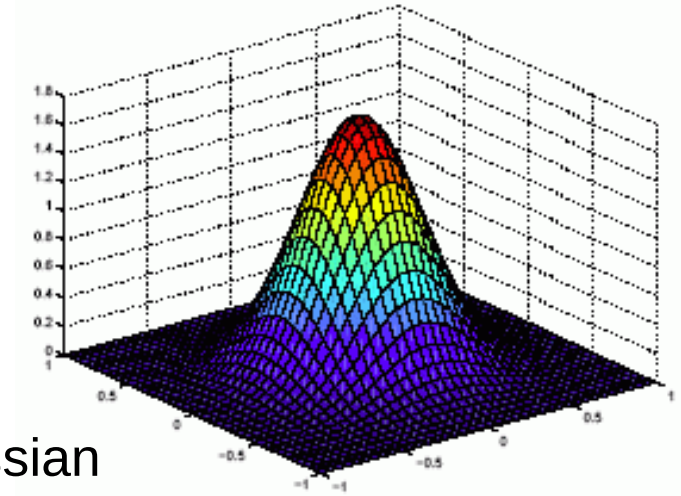
(idealized case)

Gaussian Kernel

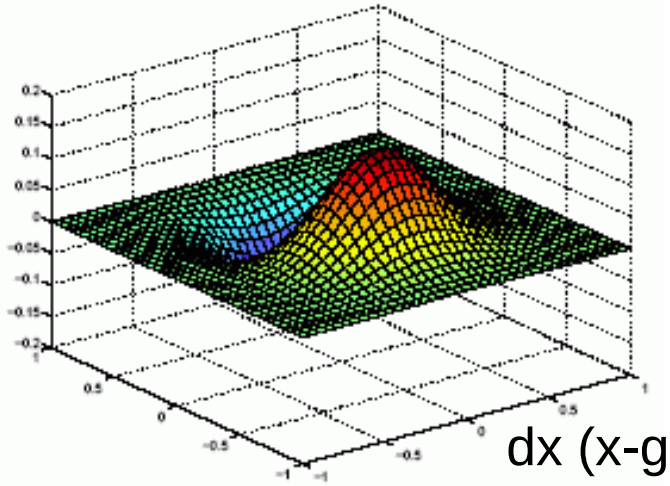
The Gaussian kernel is a popular filter function

- see book for 3x3 convolution masks

g



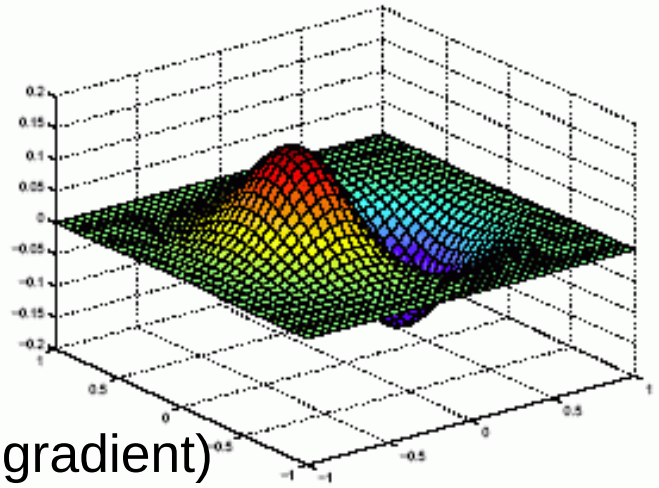
Gaussian



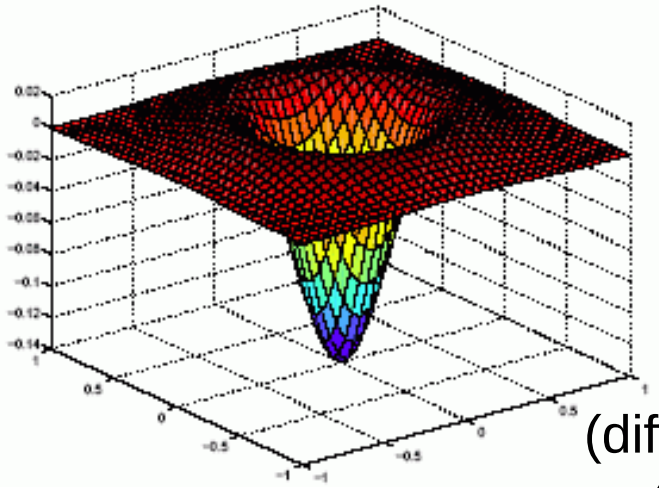
$\nabla_x g$

dx (x-gradient)

$\nabla_y g$



dy (y-gradient)



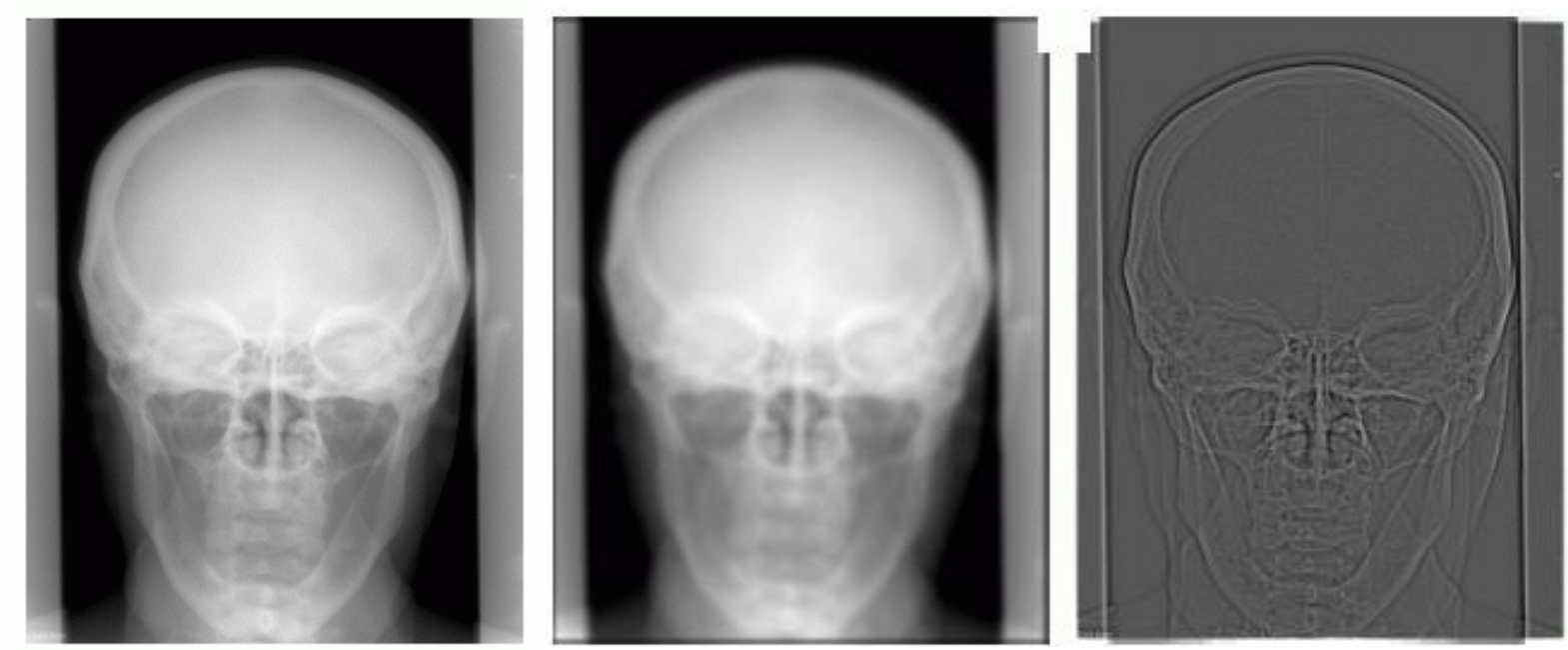
$\nabla^2 g$

Laplacian (difference of two Gaussians)

Multi-Pass Filtering: High-Pass

Several useful effects can be achieved by subsequent filtering with different masks (kernels) and/or multi-image operations

Subtracting a smoothed image from the original image leaves the edges (the high frequencies):



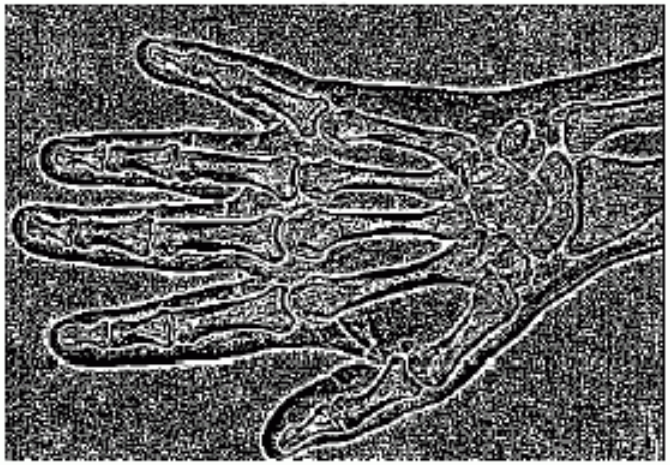
original	smoothed	original - smoothed
I	$g * I$	$I - g * I$

Multi-Pass Filtering: Unsharp Masking

Places the enhanced edges on top of a smoothed original

I

$g * I$



$I - g * I$

$g * I + (1+\alpha)(I - g * I)$

Global and Local Filtering: Shortcomings (1)

Windowing enhances contrast only for a specific range of grey levels (not sensitive to edges)

- strong edges with already good contrast are further enhanced

Edge enhancement (such as sharp masking) only boosts features within a certain frequency band

- this frequency band is determined by filter size -- features outside that band are not enhanced (cannot see many scales at the same time)
- all grey value variations (within that band) are enhanced, even if they already had good contrast

original small filter: small detail large filter: large-scale variations

Global and Local Filtering: Shortcomings (2)

One more example: digital radiograph of a foot

original

edge enhanced

window/level operation

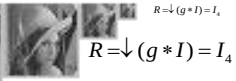
Multi-Scale Image Enhancement: Motivation

Designed to overcome these shortcomings

- enhancements will be visible at all scales at the same time
- this requires a pyramid of detail images that are added together

Image pyramid of lowpassed images

- a hierarchy of images, repeatedly lowpassed at scales of power of 2



$R = \downarrow (g * I) = I_4$

$R = \downarrow (g * I) = I_3$

$R = \downarrow (g * I) = I_2$

$R = \downarrow (g * I) = I_1$

$E = 4g * \uparrow R$

original I_0

R=reduced, *E*=expanded,
↑= upsample, ↓=downsample

Multi-Scale Image Enhancement: Detail Images

We have seen detail enhancement by high-pass filtering

- the result is called a *detail image*

We can create an image pyramid of detail images

- constructed by subtracting the smoothed image at the corresponding pyramid level from the original: $D_i = I - I_i * g$
- this gives us the detail D_i at scale i

I

$4g * \uparrow R_{i+1}$

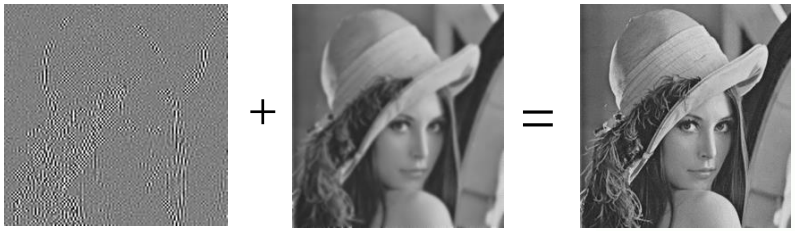
$R_{i+1} (= I_{i+1})$

D_i

Multi-Scale Image Enhancement: Detail Pyramid

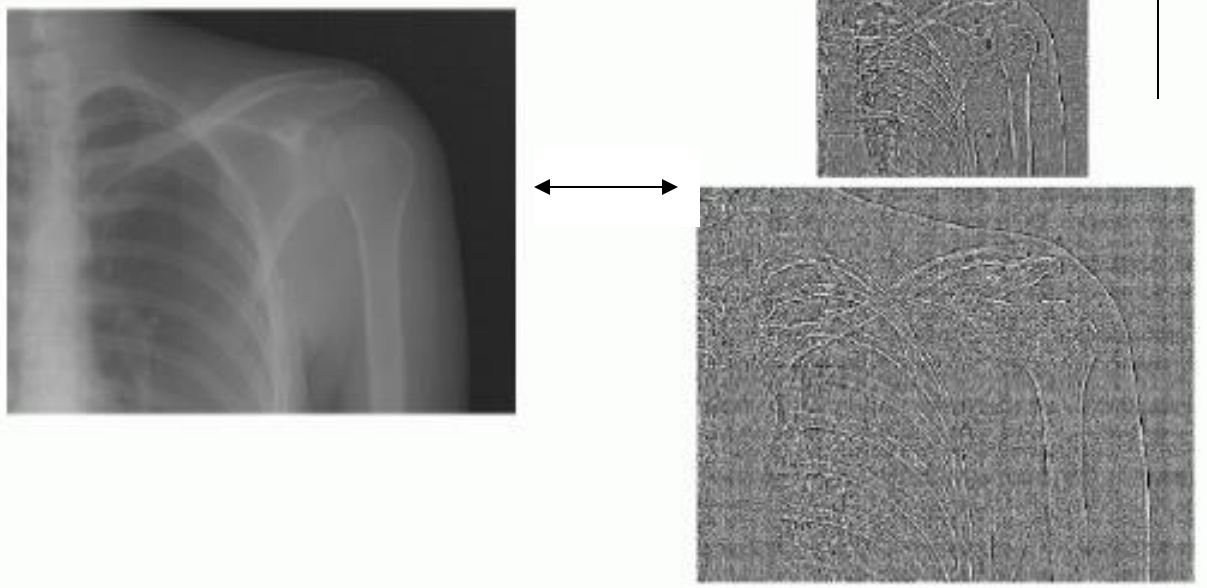
A representation of the details occuring at multiple levels of scale is called *detail pyramid*

We can reconstruct the image at level *i* by adding the expanded image at level (*i*+1) to the detail at level *i*:



$$I_i = D_i + E(I_{i+1})$$

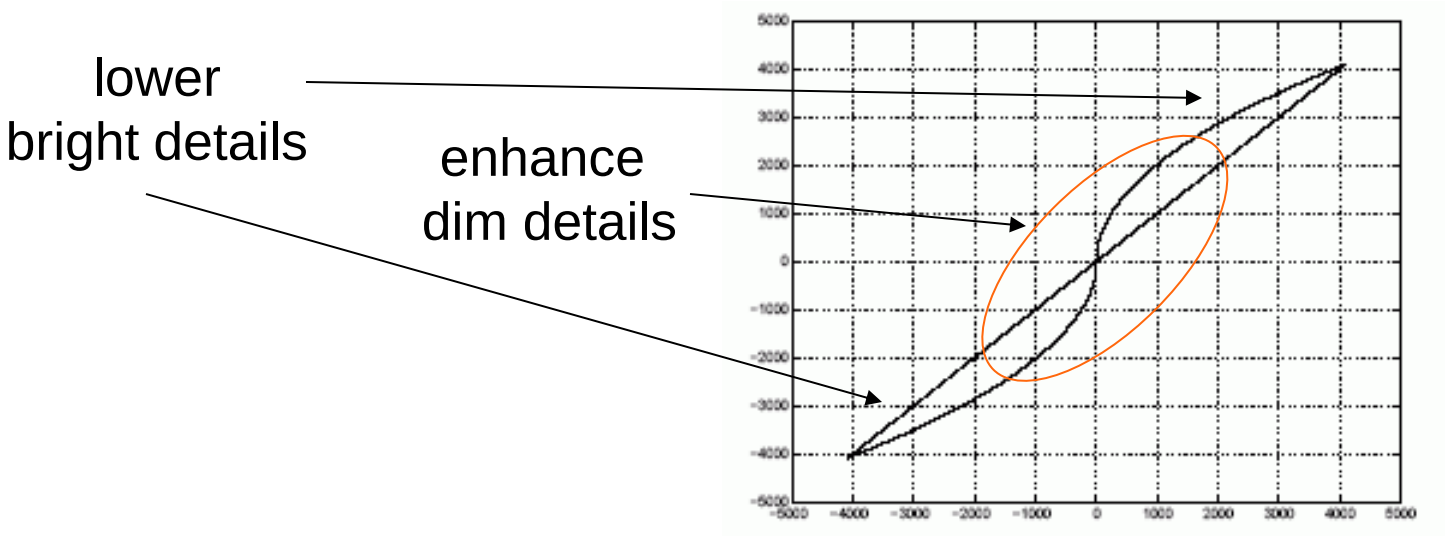
By adding all the details we can assemble the original image:



Multi-Scale Image Enhancement: Non-Linear Mapping

Strategy:

- create pyramid of detail images D_i
- apply a non-linear grey-scale transformation to each of the D_i
- this emphasizes the low-contrast details (previously invisible)
- it de-emphasizes the high-contrast details (to just noticeable levels)



- finally, re-assemble the image by adding these transformed detail images recursively

Multi-Scale Image Enhancement: Results

This strategy has been employed in the MUSICA algorithm

- developed by the company Agva Gevaert
- routinely in used in digital radiography in hospitals worldwide

edge enhanced

window/level operation

MUSICA