

Surface and Volume Based Techniques for Shape Modeling and Analysis

G. Patané¹, X. Li² and David Gu³

¹CNR-IMATI, Italy

²Louisiana State University, USA

³Stony Brook University, USA

21st November, 2013

SIGGRAPH Asia 2013 Course

Diffeomorphic registration with Large deformation using Quasi-conformal maps

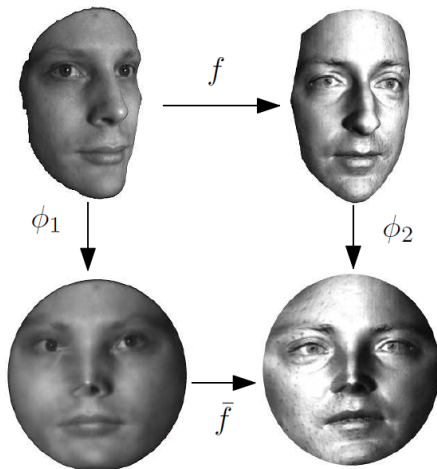
Collaborators

Ronald Lok Ming Lui, Ka Chun Lam, Chengfeng Wen and Shing-Tung Yau

- 1 Introduction
- 2 Mathematical background: QC geometry
- 3 Model 1 : Landmark-based registration
- 4 Model 2 : Landmark + intensity registration
- 5 Conclusion

Registration Framework

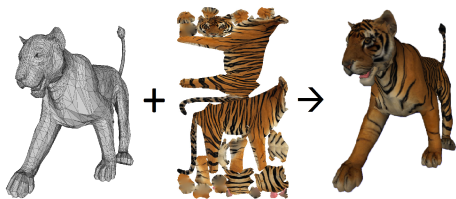
Framework



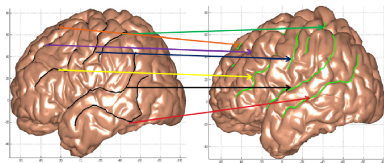
ϕ_1, ϕ_2 can be computed using Ricci flow, \bar{f} quasi-conformal mapping.

Motivation

- **Registration** : Meaningful 1-1 correspondence between data (Images, surfaces)
- **Importance** : Measure of image / surface alignment
- **Applications** : Medical shape analysis, texture mapping, video compression, etc.



Texture mapping

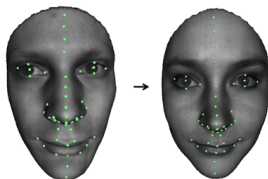


Medical registration

Intensity-based registration : Matching intensity



Landmark-based registration : Matching feature points



Landmark + intensity-based registration : Matching Both important information

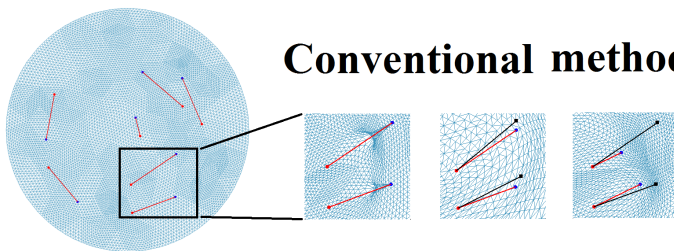
Challenges of registration

- Bijectivity cannot be guaranteed under **large deformation**
- Bijectivity cannot be guaranteed when there are **many landmark constraints**
- Huge geometric distortion
- Slow

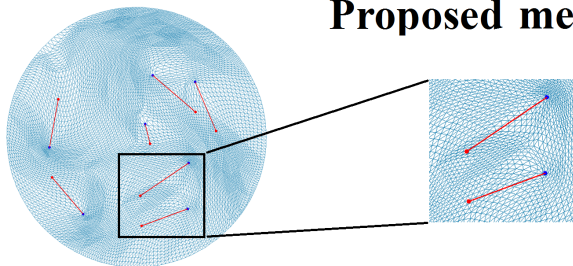
Contributions:

- **Efficiently** obtain **bijective** registration under large deformations and large number of landmark constraints.

Conventional methods

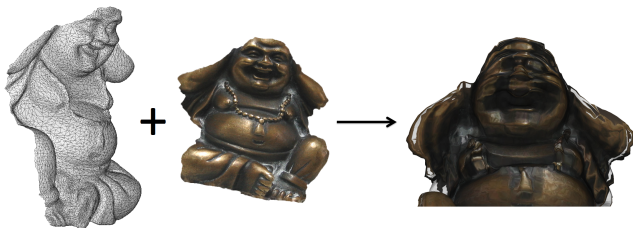


Proposed methods

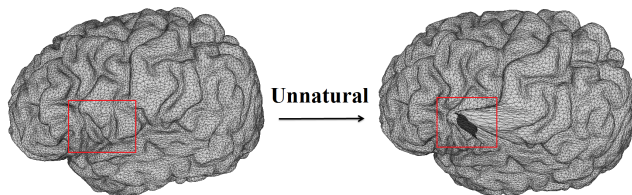


Importance of Bijectivity

Texture mapping :



Medical registration :



Mathematical background

Definition (Quasi-conformal mapping)

A function $f : \mathbb{C} \rightarrow \mathbb{C}$ is quasi-conformal if it satisfies the Beltrami equation:

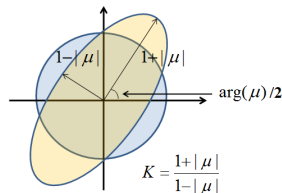
$$\frac{\partial f}{\partial \bar{z}} = \mu(z) \frac{\partial f}{\partial z} \quad (1)$$

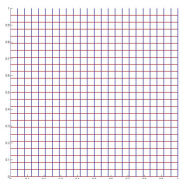
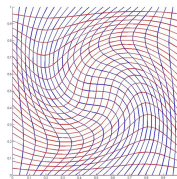
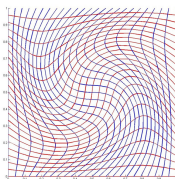
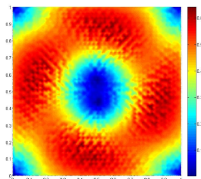
for some complex valued function μ satisfying $\|\mu\|_\infty < 1$. μ is called the Beltrami coefficients.

1-1 correspondence

Set of all
Beltrami coeff. \Leftrightarrow
 $|\mu| < 1$

Set of all
quasi-conformal
homeomorphisms
(up to Möbius transf.)



$\mu \rightarrow f$: Linear Beltrami Solver(LBS)**LBS – Reconstruct QC map f from the BC μ** Original diffeomorphism
(A)Reconstructed diffeomorphism
from Beltrami representation
(B)Beltrami representation
(C)

Recall Beltrami equation

$$\frac{\partial f}{\partial \bar{z}} = \mu(z) \frac{\partial f}{\partial z}$$

Let $f = u + iv$, where $i = \sqrt{-1}$. Then

$$\mu(f) = \frac{(u_x - v_y) + i(v_x + u_y)}{(u_x + v_y) + i(v_x - u_y)} \quad (2)$$

Substitute $\mu(f) = \rho + i\tau$ and

$$\alpha_1 = \frac{(\rho - 1)^2 + \tau^2}{1 - \rho^2 - \tau^2}; \quad \alpha_2 = -\frac{2\tau}{1 - \rho^2 - \tau^2}; \quad \alpha_3 = \frac{(1 + \rho)^2 + \tau^2}{1 - \rho^2 - \tau^2}$$

we have

$$\begin{cases} -v_y = \alpha_1 u_x + \alpha_2 u_y \\ v_x = \alpha_2 u_x + \alpha_3 u_y \end{cases} \quad (3)$$

Similarly,

$$\begin{cases} -u_y = \alpha_1 v_x + \alpha_2 v_y \\ u_x = \alpha_2 v_x + \alpha_3 v_y \end{cases} \quad (4)$$

Take divergence on both sides and let

$$A = \begin{pmatrix} \alpha_1 & \alpha_2 \\ \alpha_2 & \alpha_3 \end{pmatrix}$$

we have:

$$\nabla \cdot \left(A \begin{pmatrix} u_x \\ u_y \end{pmatrix} \right) = 0 ; \quad \nabla \cdot \left(A \begin{pmatrix} v_x \\ v_y \end{pmatrix} \right) = 0 \quad (5)$$

- Discretize \rightarrow SPD linear systems \rightarrow CG method
- Obtain x-coordinate, y-coordinate functions

Models for registration

In this talk, we introduce two models of registration using QC maps

- **Landmark-based registration using QC maps:** Obtain 1-1 correspondence based on feature landmarks.
- **Landmark and intensity based registration using QC maps:** Obtain 1-1 correspondence based on feature landmarks and intensity (such as image intensity or curvatures).

Model 1 : Landmark-based registration

Model : Landmark matching registration

Problem Solving :

$$\nu^* = \mathbf{argmin}_{(\nu)} \alpha \int |\nu|^p + \beta \int |\nabla \nu|^2 \quad (6)$$

subject to :

- $\nu^* = \mu(f)$;
- $\|\nu^*\|_\infty < 1$;
- $f(p_i) = q_i \rightarrow$ (Landmark constraints).

Idea

- BC ν controls **smoothness & bijectivity & conformality distortion**;
- **Existence of minimizer ν^*** is theoretically guaranteed (Lam-Lui, 2013).

Strategy :

Transform the problem :

$$(\nu^*, f^*) = \mathbf{argmin}_{(\nu, f)} \alpha \int |\nu|^2 + \beta \int |\nabla \nu|^2 + \gamma_n \int |\nu - \mu(f)|^2 \quad (7)$$

subject to :

- $\|\nu\|_\infty < 1$;
- $f(p_i) = q_i \rightarrow$ (Landmark constraints).

Idea :

\Rightarrow Introduce auxiliary variable f

\Rightarrow Alternate optimization over f and ν to decouple the minimization

Algorithm

$$\operatorname{argmin}_{\nu, f} \int \alpha |\nu|^2 + \beta |\nabla \nu|^2 + \gamma \int |\nu - \mu(f)|^2 \quad (8)$$

$$\Downarrow$$

A

Minimize (fixing f_n):

$$\begin{aligned} \mu_{n+1} = \operatorname{argmin}_{\nu} \int \alpha |\nu|^2 + \beta |\nabla \nu|^2 \\ + \int |\nu - \mu(f_n)|^2 \end{aligned} \quad (9)$$

B

Minimize (fixing μ_{n+1}):

$$f_{n+1} = \operatorname{argmin}_f \int |\mu_{n+1} - \mu(f)|^2 \quad (10)$$

Alternatively update μ_n and f_n using (A) and (B).

Summary of algorithm :

- Start with initial BC, ν_0 (In practice, set $\nu_0 = 0$).
- Obtain $\mu_0 = \mathbf{argmin}_\nu \alpha \int 2\nu + \beta \int |\nabla \nu|^2 + \gamma \int (\nu - \nu_0)^2$
- Use LBS to reconstruct f_0 from μ_0 satisfies landmark and boundary constraints.
- Iterate until $|\mu_{n+1} - \mu_n| \leq \epsilon$ to get the resultant map $f = f_n$.

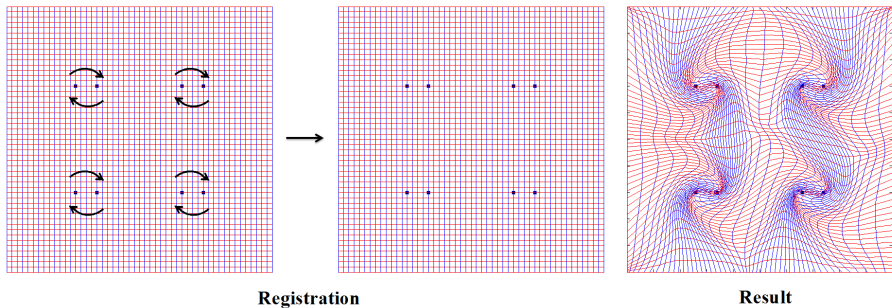
Minimization :

$$\begin{aligned} \mathbf{argmin}_{\nu} & \alpha \int |\nu|^2 + \beta \int |\nabla \nu|^2 + \gamma \int (\nu - \nu_0)^2 \\ \Rightarrow & \alpha \int 2\nu + \beta \int \Delta \nu + \gamma \int 2(\nu - \nu_0) = 0 \\ \Rightarrow & \nu = 2\gamma(\beta\Delta + 2\alpha I + 2\gamma I)^{-1}\nu_0 \\ \Rightarrow & \text{Solve a linear system} \end{aligned} \tag{11}$$

Experimental result: Landmark matching registration

Landmark matching example(1)

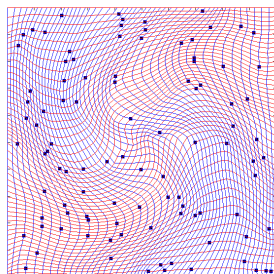
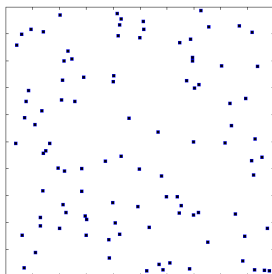
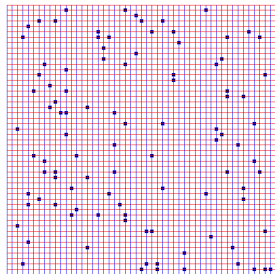
Matching eight points



Animation

Landmark matching example(2)

Matching 100 points



Registration

Result

Animation

Model : Extremal problem

Problem Solving :

$$\nu^* = \mathbf{argmin}_{(\nu)} \{ \|\nu\|_{\infty} \} \quad (12)$$

subject to :

- $\nu^* = \mu(f)$;
- $\|\nu^*\|_{\infty} < 1$;
- $f(p_i) = q_i \rightarrow$ (Landmark constraints).

Idea

- Replace the energy functional by L^{∞} -norm of the Beltrami coefficient;
- The problem is equivalent to finding the **extremal or Teichmüller map**.

Definition (Extremal mapping)

Let $f : S_1 \in \mathbb{C} \rightarrow S_1 \in \mathbb{C}$ be a quasi-conformal mapping between S_1 and S_2 . f is said to be an extremal mapping if for any quasi-conformal mapping $h : S_1 \rightarrow S_2$ isotopic to f relative to the boundary,

$$\|\mu(f)\|_\infty \leq \|\mu(h)\|_\infty \quad (13)$$

It is uniquely extremal if the inequality is strict.

Extremal mapping = Quasi-conformal map with
least conformality distortion

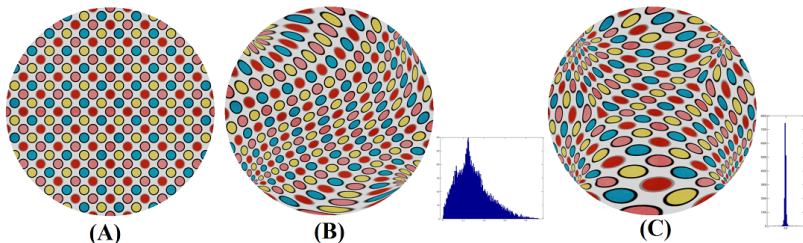
Teichmüller extremal mapping (T-map)

Definition (Teichmüller mapping)

Let $f : S_1 \in \mathbb{C} \rightarrow S_2 \in \mathbb{C}$ be a quasi-conformal mapping between S_1 and S_2 . f is said to be an Teichmüller mapping associated with $\varphi : S_1 \rightarrow \mathbb{C}$ if its associated Beltrami coefficient is of the form:

$$\mu(f) = k \frac{\bar{\varphi}}{|\varphi|} \quad (14)$$

for some constant $k < 1$ and $\varphi \neq 0$.



Definition (Extremal mapping)

Let $f : S_1 \in \mathbb{C} \rightarrow S_1 \in \mathbb{C}$ be a quasi-conformal mapping between S_1 and S_2 . f is said to be an extremal mapping if for any quasi-conformal mapping $h : S_1 \rightarrow S_2$ isotopic to f relative to the boundary,

$$\|\mu(f)\|_\infty \leq \|\mu(h)\|_\infty \quad (15)$$

It is uniquely extremal if the inequality is strict.

Extremal mapping = Quasi-conformal map with
least conformality distortion

Relation:

Under suitable boundary cond.

$(h' \neq 0 \text{ and } |h''| < C)$

T-map = Unique Extremal map

Properties of T-maps:

- Minimal conformal distortion
- Uniqueness
- Bijectivity

Extended model : T-maps

Computing T-map

Problem Solving:

Find $f : S_1 \rightarrow S_2$ such that

$$\frac{\partial f}{\partial \bar{z}} = k \frac{\bar{\varphi}}{|\varphi|} \frac{\partial f}{\partial z} \quad (16)$$

and satisfies

- $0 \leq k < 1$ and $\varphi : S_1 \rightarrow \mathbb{C}$ holomorphic;
- $f|_{\partial S_1} : \partial S_1 \rightarrow \partial S_2 = g$ (Boundary condition);
- $f(p_i) = q_i, i = 1, \dots, N$ (Landmark constraints).

Mathematical formulation of finding T-map

$$(\nu, f) = \mathbf{argmin}_{\nu: S_1 \rightarrow \mathbb{C}} \{ \|\nu\|_\infty \} \quad (17)$$

subject to:

- $\nu = \mu(f)$;
- $\nu(f) = k \frac{\bar{\varphi}}{|\varphi|}$ where $0 \leq k < 1$ and $\varphi : S_1 \rightarrow \mathbb{C}$ holomorphic;
- $f|_{\partial S_1} = g$ (boundary condition);
- $f(p_i) = q_i, i = 1, \dots, N$ (Landmark constraints).

Idea:

- **Find a path:** Initial BC $\nu_0 \rightarrow$ unique BC ν of Teichmüller type.
- **Two crucial properties** of a extremal T-map:
 - (P1) $\mu = k \frac{\bar{\varphi}}{|\varphi|}, 0 \leq k < 1, \varphi : S_1 \rightarrow \mathbb{C}$ holomorphic.
 - (P2) $\mu = \mathbf{argmin}_{f: S_1 \rightarrow S_2} \{ \|\mu(f)\|_\infty \}$, where f satisfies the given boundary and landmark constraints.

QC-iteration

- Start with an initial map f_0 whose BC is $\nu_0 := \mu(f_0)$.
- Project ν_0 to a BC of constant norm and perform Laplace smoothing on $\arg(\nu_0) \rightarrow \mu_1$. (Property 1)
- **LBS** reconstructs f_1 from μ_1 . satisfies boundary and landmark constraints.
- Iterate until f_n converges to the unique extremal T-map. (Property 2)

Projection onto Teichmüller type

Consider $\mu = k \arg(\nu_0)$,

Aim :

- $\nu_0 \rightarrow \mu := k \arg(\nu_0)$
- k decreases in each iteration

A natural choice:

$$k = \mathcal{A}(\nu_0) := \frac{\int_{S_1} |\nu_0| dS_1}{\text{Area}(S_1)} \quad (18)$$

- When $\nu_0 \neq$ Teichmüller type $\rightarrow k < \|\nu_0\|_\infty$
- When $\nu_0 =$ Teichmüller type $\rightarrow k$ unchanged.

Holomorphic property of φ

Aim : Optimal ν : $\arg(\nu) = \frac{\bar{\varphi}}{|\varphi|}$

Consider: $\varphi = |\varphi|e^{i\theta}$ and $\nu = |\nu|e^{i\theta}$

$$\log \varphi = \log |\varphi| + i\theta \Rightarrow \theta \text{ harmonic} \Rightarrow \Delta \theta = 0$$

\Rightarrow Laplace smoothing on θ in each iteration

$$\mathfrak{L}(\nu_0)(T) = |\nu_0(T)| \left(\sum_{T_i \in \text{Nbhd}(T)} \frac{\arg(\nu_0(T_i))}{|\text{Nbhd}(T)|} \right) \quad (19)$$

Optimal state:

θ harmonic

$\rightarrow \zeta$ harmonic conjugate of θ

$\rightarrow \varphi = e^{\zeta - i\theta}$.

Convergence of the QC-iteration

Theorem (Convergence of the QC iteration, Lui-Gu-Yau, 2013)

The QC iteration gives a convergent sequence of pairs (f_n, ν_n) , where ν_n is the Beltrami coefficient of f_n , whose limit point is (f^, ν^*) . Here, ν^* is the unique admissible Beltrami coefficient of Teichmüller type associated with the extremal Teichmüller map.*

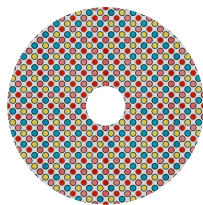
K.C. Lam, X.F. Gu, S.T. Yau, L.M. Lui, "Teichmüller mapping (T-Map) and its applications to landmark matching registrations", SIAM Journal on Imaging Sciences (2013)

Experimental result: T-Maps

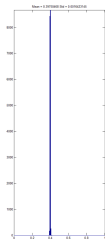
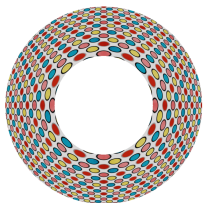
T-maps example(1)

Analytic example : Ring with inner and outer radii r_0 and r_1 to ring with inner and outer radii r'_0 and r'_1 .

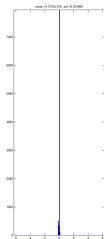
Corresponding maximal dilation $K = \frac{1+\|\mu\|_\infty}{1-\|\mu\|_\infty} = \frac{\ln(r'_1/r'_0)}{\ln(r_1/r_0)}$



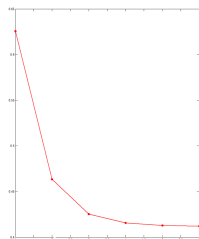
(A)



(B)



(C)

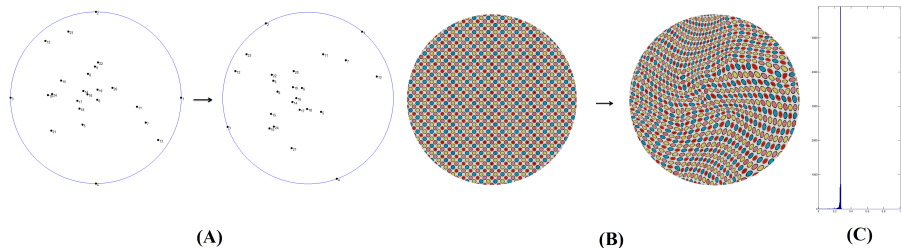


(D)

Take $r_0 = r'_0 = 1$ and $r_1 = 0.2$, $r'_1 = 0.5$, error of $K = 0.0013219$.

T-maps example(2)

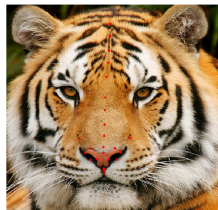
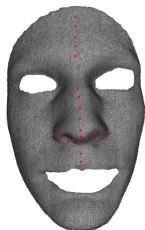
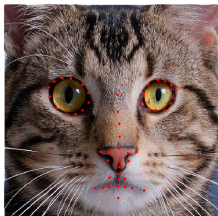
Example 2 : 4-point boundary constraints + 24 interior landmark constraints enforced.



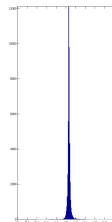
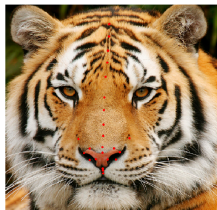
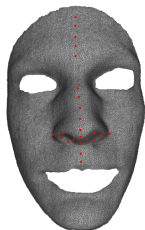
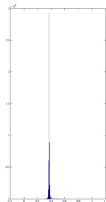
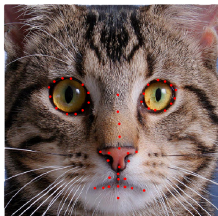
- (A) 24 landmark constraints
- (B) T-map
- (C) Histogram : $|\mu|$ of T-map

Applications

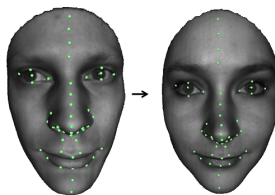
Constrained texture mapping



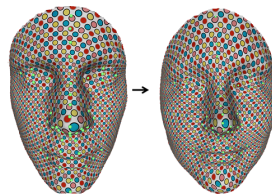
Constrained texture mapping



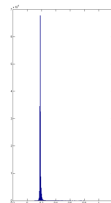
Face registration



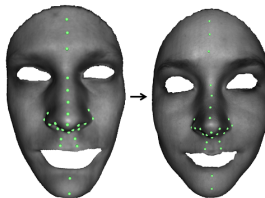
(A)



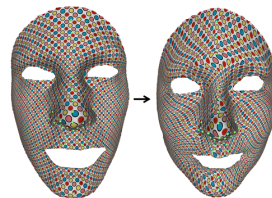
(B)



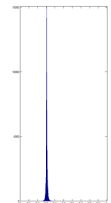
(C)



(A)

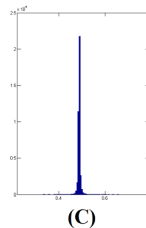
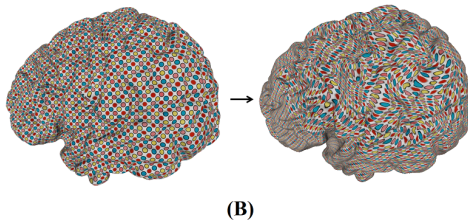
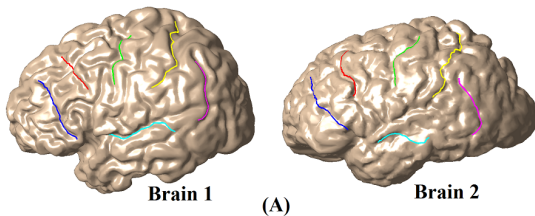


(B)



(C)

Medical registration : Brain



Model 2 : Landmark + intensity registration

Model : Landmark + intensity registration

Problem Solving :

$$(\nu^*, f^*) = \mathbf{argmin}_{(\nu, f)} \alpha \int |\nu|^p + \beta \int |\nabla \nu|^2 + \gamma \int (I_1 - I_2(f))^2 \quad (20)$$

subject to :

- $\nu^* = \mu(f^*)$;
- $\|\nu^*\|_\infty < 1$;
- $f^*(p_i) = q_i \rightarrow$ (Landmark constraints).

Idea

- BC μ controls **smoothness & bijectivity & conformality distortion**;
- $\int (I_1 - I_2(f))^2$ controls the sum of squared difference (SSD) of the intensity difference in the two data.

Algorithm

Use penalty method to minimize :

$$(\nu^*, \mu^*) = \mathbf{argmin}_{\mu, \nu} \alpha \int |\nu|^2 + \beta |\Delta \nu|^2 + \frac{1}{\sigma^2} |\nu - \mu|^2 + \gamma \int (I_1 - I_2(f^\mu))^2 \quad (21)$$

subject to :

- $\|\nu^*\|_\infty < 1$;
- $f^{\mu^*}(p_i) = q_i \rightarrow$ (Landmark constraints).

Idea :

\Rightarrow Introduce auxiliary variable μ

\Rightarrow Alternate optimization over μ and ν to decouple the minimization

Algorithm

$$\operatorname{argmin}_{\mu, \nu} \int \alpha |\nu|^2 + \beta |\nabla \nu|^2 + \frac{1}{\sigma^2} |\nu - \mu|^2 + \int \gamma (I_1 - I_2(f^\mu))^2 \quad (22)$$

$$\Downarrow$$

A

Minimize :

$$\begin{aligned} \mu_{n+1} = \operatorname{argmin}_{\mu} & \gamma \int (I_1 - I_2(f^\mu))^2 \\ & + \frac{1}{\sigma_n^2} |\mu - \nu_n|^2 \end{aligned} \quad (23)$$

B

Minimize :

$$\begin{aligned} \nu_{n+1} = \operatorname{argmin}_{\nu} & \int \alpha |\nu|^2 + \beta |\nabla \nu|^2 \\ & + \frac{1}{\sigma_n^2} |\nu - \mu_{n+1}|^2 \end{aligned} \quad (24)$$

Alternatively update μ_n and ν_n using (A) and (B).

Minimization A

Strategy : Gradient descent

Note that :

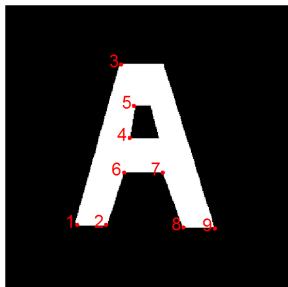
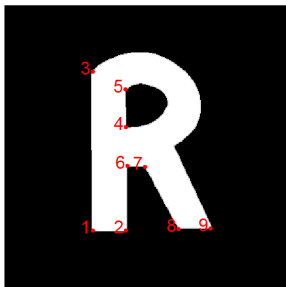
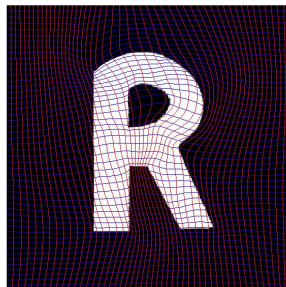
$$\begin{aligned}
 \frac{\partial(f + df)}{\partial \bar{z}} &= (\mu + d\mu) \frac{\partial(f + df)}{\partial z} \\
 \Rightarrow \frac{\partial f}{\partial \bar{z}} + \frac{\partial df}{\partial \bar{z}} &= \mu \frac{\partial f}{\partial z} + d\mu \frac{\partial df}{\partial z} + \mu \frac{\partial df}{\partial z} + d\mu \frac{\partial df}{\partial z} \\
 \Rightarrow d\mu &= \frac{\frac{\partial df}{\partial \bar{z}} - \mu \frac{\partial df}{\partial z}}{\frac{\partial f}{\partial z}}
 \end{aligned} \tag{25}$$

Gradient descent direction of BC from $\int (I_1 - I_2(f^\mu))^2$ can be obtained.

Gradient descent direction of BC from $|\mu - \nu_n|^2$ is $2(\mu - \nu_n)$.

Synthetic example(1)

Alphabet "A" to alphabet "R"

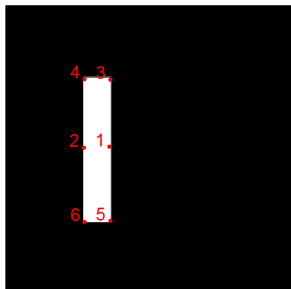
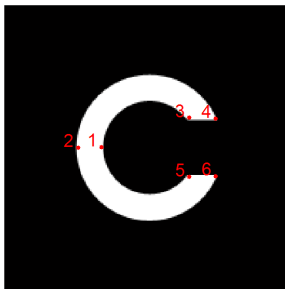
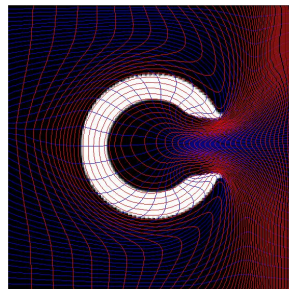
**Moving****Fixed****Result**

Synthetic example(1)

Animation

Synthetic example(2)

Alphabet "I" to alphabet "C"

**Moving****Fixed****Result**

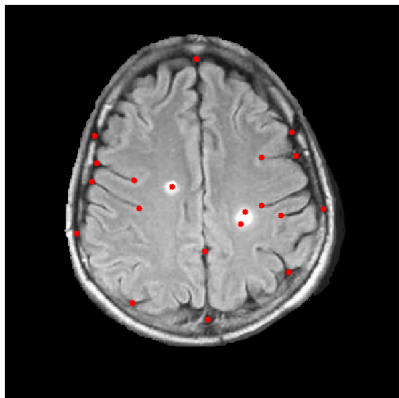
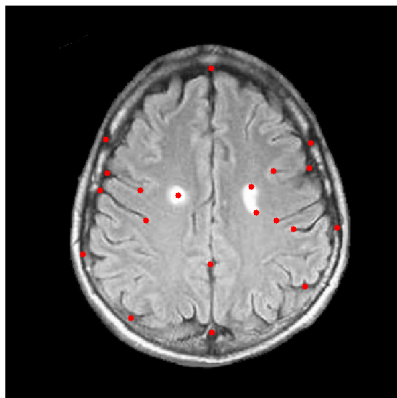
Synthetic example(2)

Animation

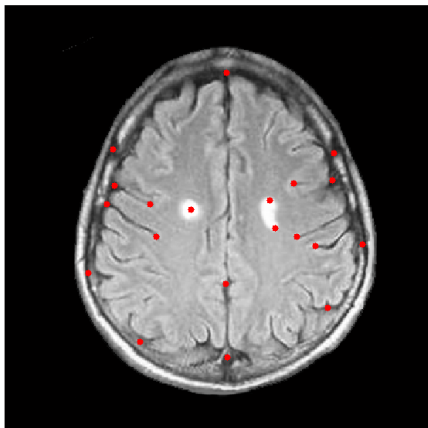
Applications

Image registration : Brain MRI

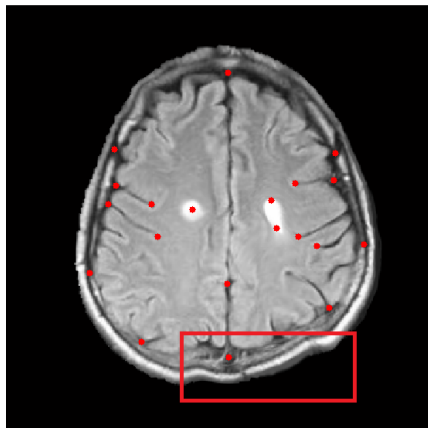
Registration problem :

**Moving****Target**

Landmark only :

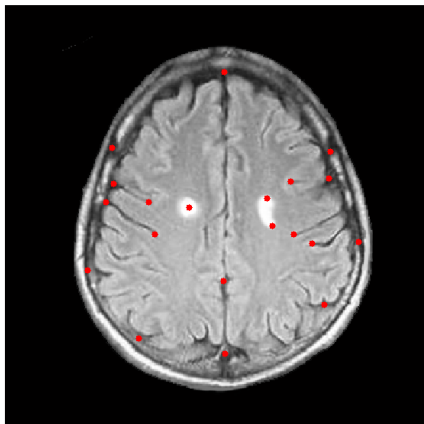


Target

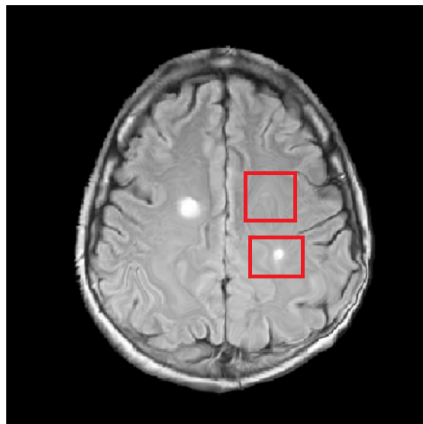


Landmark

Intensity only :

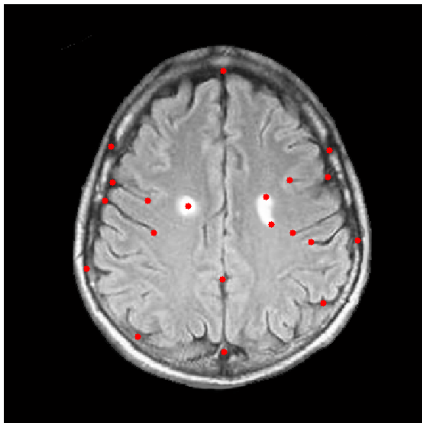


Target

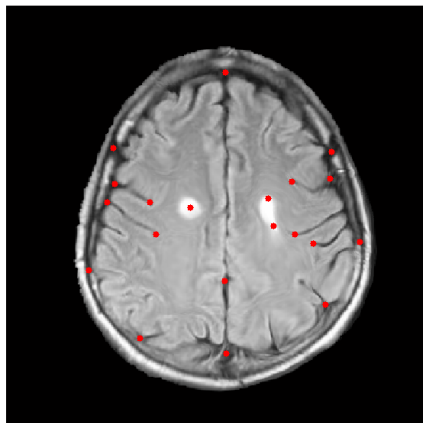


Intensity

Landmark + intensity only :



Target



**Landmark +
intensity**

Image registration : X-ray bone



Landmark only :

**Target****Landmark**

Intensity only :

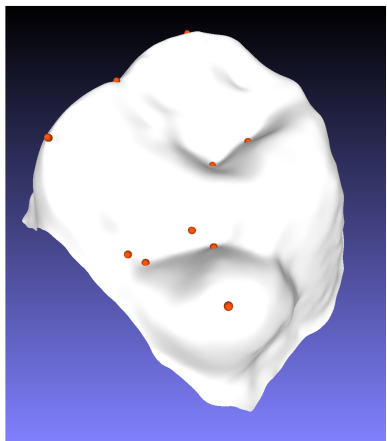
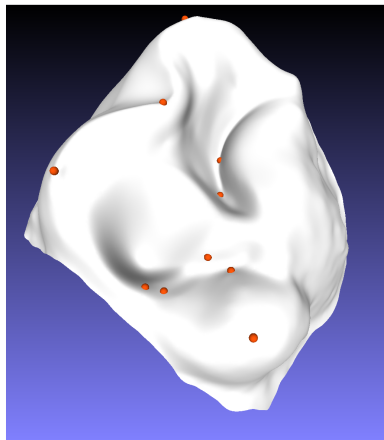
**Target****Intensity**

Landmark + Intensity :

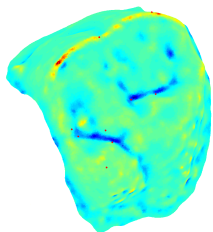
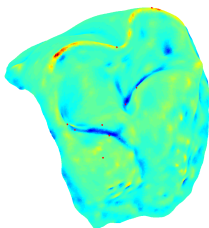
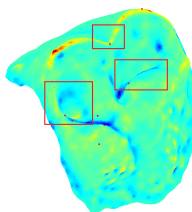
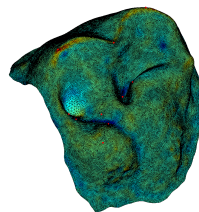
**Target****Intensity +
Landmark**

Surface registration : Teeth

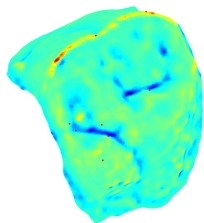
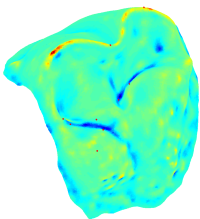
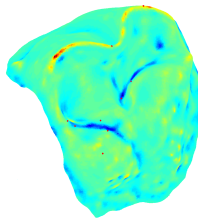
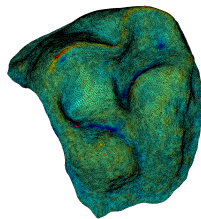
Teeth registration

**Teeth 1****Teeth 2**

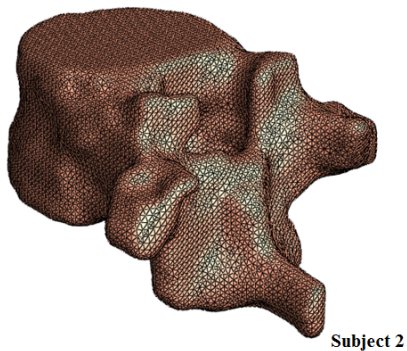
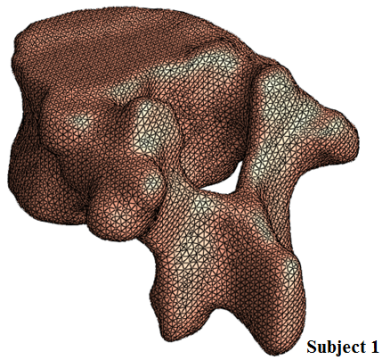
Landmark matching only

**Moving****Fixed****Registration result**

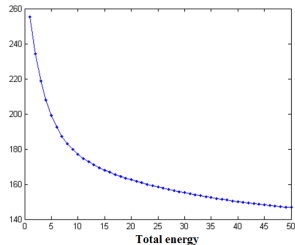
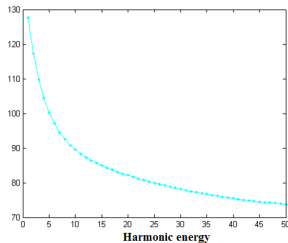
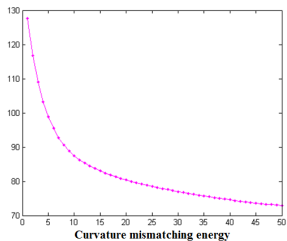
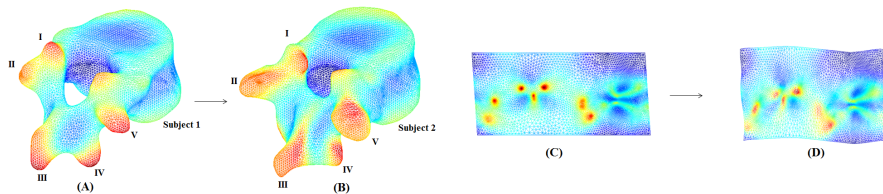
Landmark + intensity matching

**Moving****Fixed****Registration result**

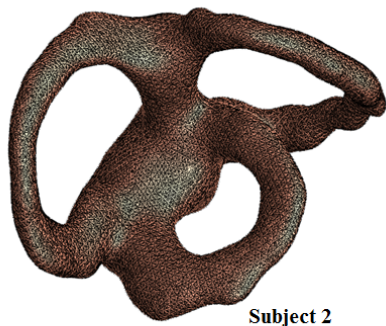
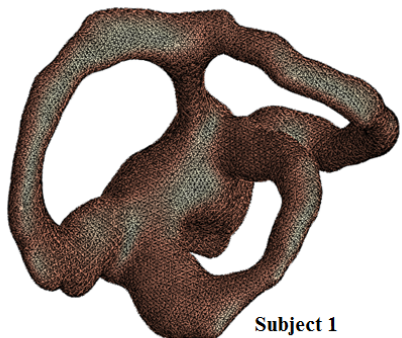
Medical registration : Vertebral bone

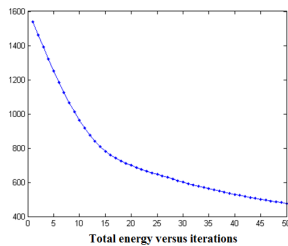
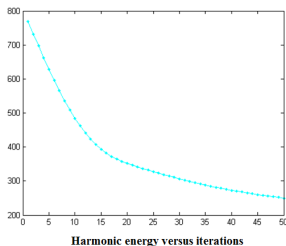
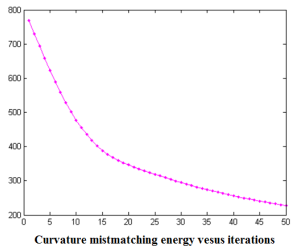
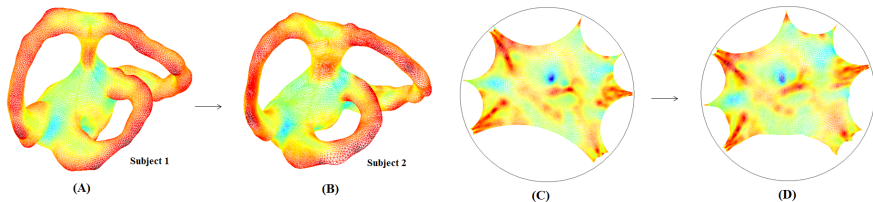


Registration result:



Medical registration : Vestibular system





Conclusion

- Propose Landmark registration algorithm.
- Extend to obtain T-maps and show further application.
- Propose Landmark + intensity registration algorithm.
- Extension to high-genus surface registration and show further application.

Thank You